Multiscale Motion Mapping – A Novel Computer Vision Technique for Quantitative, Objective Echocardiographic Motion Measurement Independent of Doppler

First Clinical Description and Validation

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Abstract

Background— Objective, quantitative, segmental noninvasive/bedside measurement of cardiac motion is highly desirable in cardiovascular medicine, but current technology suffers from significant drawbacks, such as subjectivity of conventional echocardiographic reading, angle dependence of tissue Doppler measurements, radiation exposure by computer tomography, and infrastructure requirements in magnetic resonance imaging. We hypothesized that Computer Vision technology could represent a powerful new paradigm for quantification in echocardiography.

Methods and Results— We present Multiscale Motion Mapping, a novel computer vision technology that is based on mathematical image processing and that exploits echo information in a fashion similar to the human visual system. It allows Doppler- and border-independent determination of motion and deformation in echocardiograms at arbitrary locations.
Correctness of the measurements was documented in synthetic echoes and phantom experiments. Exploratory case studies demonstrated its usefulness in a series of complex motion analyses including abnormal septal motion and analysis of myocardial twisting. Clinical applicability was shown in a consecutive series of echocardiograms, where good feasibility, good correlation with expert rating, and good intra- and interobserver concordance were documented. Separate assessment of two-dimensional displacement and deformation at the same location was successfully applied to elucidate paradoxical septal motion, a common clinical problem.

Conclusions— This is the first clinical report of Multiscale Motion Mapping, a novel approach to echocardiographic motion quantification. For the first time, full 2D echocardiographic assessment of both, motion and deformation is shown to be feasible. Overcoming current limitations, this computer vision-based technique opens a new door to objective analysis of complex heart motion.

Key Words: imaging, echocardiography, myocardial contraction, ischemia, infarction

Condensed Abstract

Reliable, noninvasive assessment of cardiac motion is critical in ischemic heart disease and heart failure, but in current clinical practice, subjective, semiquantitative assessment still dominates. This report describes a novel approach to quantitative, objective assessment of cardiac motion and deformation based on principles of computer vision; it explores the validity of this approach and assesses its applicability in clinical practice. For the first time in echocardiography, full 2D assessment of motion and deformation by echocardiography has become feasible, opening a new door to comprehensive, objective analysis of cardiac function.

Introduction

Although the title of the very first description of echocardiography by Edler and Hertz in 1954 mentioned "recording of the movements of heart walls" as its goal[1], measuring wall motion objectively and quantitatively has remained difficult in clinical practice. Objective assessment of wall motion is of considerable importance in a broad range of patients: the objective documentation that contractility is normal in patients examined in a screening situation may be as important as the reliable quantification of ventricular function in heart failure and the detection of wall motion abnormalities at rest or stress in those with suspected ischemic heart disease. The presence of segmental variations in contractility adds an additional level of difficulty to this analysis. The causes of these difficulties are manifold: Cardiac motion is complex, encompassing active thickening, passive translation of contracting and non-contracting segments, rotational components (e.g., apical twisting) as well as shear components, for example, between endocardial, epicardial and pericardial structures. Furthermore, ultrasound images are typically noisy, tissue intensities are not constant and endocardial borders lack continuity, thus significantly limiting the applicability of standard image analysis approaches such as border detection algorithms. The most successful current technique, tissue Doppler-based analysis of motion[2-5] and deformation[6-8], is hampered by the critical dependence of both measurements from the ultrasound beam direction, leading to signal dropout and velocity underestimation. However, most cardiologists will agree that the human visual system is quite apt at seeing such complex motion patterns even in noisy data, although analysis remains subjective and semi-quantitative. We hypothesized that application of some of the fundamental properties of the human visual system to echo quantification could result in robust quantification of motion in an objective manner. To this end, we developed and validated Multiscale Motion Mapping, a computer vision based approach to echocardiographic motion quantification.

Methods

Multiscale Motion Mapping is a computer vision technology based on advanced mathematical image data analysis. The information contained in echocardiographic loops can be exhaustively described as a large numerical dataset usually rendered as an image sequence on a screen; it is used here for computation of local motion and deformation. The following method description is given for the non-mathematician, while mathematical details of the approach are given in a separate technical paper in an engineering journal[9]. The technique has a number of key features:

Continuous representation of reality: Conventional echocardiographic technology including Doppler echo rests on pixel- and frame-wise image processing: Data for each pixel is computed independently and the overall frame is then composed from the individual pixels, after which the next frame is computed. In contrast, real objects are smoothly connected in space and move continuously instead of jumping from frame to frame. Therefore, we use a continuous and coherent mathematical representation in space and time, a so-called spline model[10] of the ultrasound data, an approach of proven value in other fields.

Multiresolution strategy: Human vision is strongly context dependent: The overall structure of an object determines which details our brain will expect and recognize, while apparent features that are incoherent with the larger context are suppressed: e.g., when looking at a partner's face in heavy snowfall, we will pay more attention to the overall facial expression than to some bright snowflakes in front of the face. In addition, our brain expects moving objects to be coherent in time, making human vision even more robust. We therefore implemented spatial context dependence and temporal coherence in a so-called multiresolution pyramid: overall shape and coarse motion are used to refine the analysis of smaller structures and of more detailed motion in a recursive fashion, analogous to the hierarchical organization of the early image processing stages in the human visual system.

Affine model of motion: Typical motion in echocardiograms includes translation, deformation (e.g., myocardial shortening along the myocardial fiber axis accompanied by thickening of the same structure perpendicular to the fiber axis), rotation (e.g.,

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valvular motion, apical twisting), and shear motion (e.g., inner versus outer myocardial planes, epicardium versus pericardium). Mathematically, all these motion patterns (Figure 1) can be locally described in a so-called *affine model*:

$$
\begin{pmatrix} u(x,y) \\ v(x,y) \end{pmatrix} = \underbrace{\begin{pmatrix} u_0 \\ v_0 \end{pmatrix}}_{\substack{\text{Trans-}\\\text{lation}}} + \underbrace{\begin{pmatrix} u_x & u_y \\ v_x & v_y \end{pmatrix} \cdot \begin{pmatrix} x - x_0 \\ y - y_0 \end{pmatrix}}_{\text{Rotation and deformation}}
$$

Equation 1: *Mathematical formulation of the affine motion model.*
Local motion (u, v) at each location is determined by translation (u_0, v_0) at region center (x_0, y_0) and local rotation and deformation coded by derivatives u_x, u_y, v_x, v_y. The image region is chosen of such size that it contains enough information to solve this equation for all unknowns using linear algebra.

At the heart of Multiscale Motion Mapping is the insight that for each image region in an echocardiogram, knowledge of the numerical grayscale values in this region (readily available in the image raw data) is sufficient for computation of just that affine motion equation that fits best to this region, thereby predicting local translation, rotation and deformation. This ability of Multiscale Motion Mapping to fit complex heart motion is one of several differences to conventional "optical flow" techniques, to which it is superior[9].

Motion visualization: Multiscale Motion Mapping yields a large amount of motion information. A simple, intuitive display is therefore of particular importance. With simple mouse clicks, different motion representations can be displayed (Figure 2):

a) An arrow representation of 2D velocity at arbitrary locations and time points (Figure 2a). The arrow direction corresponds to the motion direction; the arrow length codes the absolute velocity. Their numerical values can also be exported.

b) Radial velocity towards a reference point displayed as a color map. This color map is Doppler-independent and thus free of the angle dependent dropouts typical for the latter. Radial inward motion can be represented in the same color independent of the ultrasound beam angle, rendering motion display more intuitive.

c) Active myocardial contraction has two physiologic components: shortening along the myocardial fiber direction, and thickening perpendicular to it. Both can be represented in an ellipse that indicates the two principal axes and the absolute values of 2D strain rate, circumventing the problem of tissue Doppler where the two strain rate components will cancel each other at certain beam angles.

Echocardiograms were acquired with a Philips SONOS 5500 in native digital format or with one of several DICOM-3 enabled machines from Siemens, General Electrics, Toshiba, and were stored digitally. Processing was done on a standard PC, with key hardware requirements consisting either of a current Pentium IV or PowerPC G4 processor and 1 Gigabyte of RAM, with processing times in the range of one minute.

Validation experiments: Validation of measured versus true motion was first performed in two setups for which true motion is known: a) synthetic echo sequences and b) moving physical phantoms. Then, clinical exploration was done with a series of prototypical echocardiograms. At last, the feasibility of the method in routine echo was evaluated in a consecutive series of echocardiograms performed for clinical indications. Here, conventional subjective reading was done by three experts. The 16-segment nomenclature[11] was used, assigning to each segment one of 5 subjective ratings from "hyper-" to "dyskinetic" and giving each view an overall label as "normal" (hyper-, normokinetic) or "abnormal" (hypo-, a-, dyskinetic). Objective analysis by Multiscale Motion Mapping was performed by two blinded observers, as well as by repetition of the measurements by the same observer after several weeks. Velocity measurements and subjective ratings were used to train an artificial neural network (three-layer structure, sigmoid response, error-backpropagation algorithm for training[12]) using the first half of the available data. The ability for automatic classification of patients as normal or abnormal using quantitative measurements was validated using the second half of the data.

Standard statistical methods were used with a two-sided significance level of 0.05. Linear regression and Bland-Altman Analysis[13] were used to compare measured with correct motion in models with known motion. Interobserver agreement and

intraobserver consistency were assessed using Bland-Altman analysis for continuous variables and using the Kappa test for classification.

Results

In the following section, we present results obtained from synthetic ultrasound data, phantom experiments and clinical echocardiograms. Motion can only be displayed for single frames in this print version; for a better dynamical perception, moving image loop representations can be viewed at

http://bigwww.epfl.ch/suehling/research/MMMdemo.html .

Overall capabilities in synthetic echocardiograms

Multiscale Motion Mapping was first applied to synthetic echo loops to assess its capabilities in the case of simplified, clearly defined motion. The example shown in Figure 3(a) simulates an apical short axis view. The applied motion consists of uniform radial expansion/contraction combined with global, periodic translation in diagonal direction. The capabilities of the algorithm to measure and visualize this motion are demonstrated in Figure 3(b)-(d). The following representations were computed from a 2D grayscale loop:

a) A full motion field indicating velocity arrows at all locations and all time points in an image loop is shown in Figure 3(b). The arrow display reflects the superposition of radial contraction and global translation.

b) A color map indicating motion components relative to the ventricular centroid moving with the ventricle Figure 3(c). The yellow/red color indicates uniform inward motion.

c) Figure 3(d) displays 2D deformation by strain rate ellipses. Myocardial thickening and circumferential shortening is indicated by the ellipses. The deformation map is independent from the underlying translational motion. In contrast to tissue Doppler-based strain rate analysis, deformation measurement does not depend on the deformation orientation.

Measured velocities were compared to known true motion and showed very good agreement. In Bland-Altman analysis, there was a minimal bias (mean velocity difference: -0.005 pixel/frame, $p<0.001$, SD=0.056 pixel/frame (1.4% of measured range)) with a correlation coefficient of 1.00 ($p<0.001$; regression line: $y = 1.04x - 0.00$), documenting the correctness of the algorithm. Measured deformation also

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corresponded well to true deformation (for absolute strain rate, correlation coefficient 0.88 (p<0.001), mean difference 0.0 s^{-1} (p=NS); SD= 4.4% of measured range; correlation coefficient for strain rate direction 0.89, p<0.001).

Phantom experiment

The ability to analyze motion in real ultrasound data was tested in a phantom experiment. A cylinder shaped, tissue-mimicking phantom (radius: 4.0 cm) was placed inside a tube of water and rotated with constant angular velocity (1.1 rad/s). Figure 4(a) and (b) show one frame of the B-mode sequence and its rotational velocities, respectively. For comparison, the color Doppler signal is shown in Figure 4(c); here, the typical Doppler signal dropout at certain beam angles is evident. Estimated velocities were in good agreement with true phantom motion. The correlation coefficient between true and estimated velocity magnitudes was 0.97 (p<0.001; regression line: y = 0.86x – 0.01). Bland-Altman analysis showed a negligible bias (mean velocity difference: 0.108 cm/s, p<0.001, SD=0.292 cm/s (3.3% of the measured range)).

Application to clinical echocardiograms

The ability to display motion in clinical echocardiograms independent from the ultrasound beam angle is demonstrated in the short axis view of a normal beating heart shown in Figure 5(a). The ability of Multiscale Motion Mapping to assess apical myocardial twisting, which is clearly appreciated visually, is illustrated in Figure 5(b) using the arrow display. The motion arrows document the clock-wise apical twisting during early diastole. The complexity of the actual motion pattern becomes readily apparent in the fish-swarm like appearance of the arrows, illustrating the difficulties of motion assessment with conventional methods that are limited to detecting a 1D motion component only.

The color-coded radial velocity component towards the center point is shown in Figure 5(c) for mid-systole and in Figure 5(d) for early diastole. Note that in systole, the entire circumference is color-coded in red, indicating inward motion everywhere (while in tissue Doppler, there would be a whole spectrum of colors, rendering reading less straightforward).

Deformation maps of the myocardium during systole and diastole are shown in Figure 5(e) and (f), respectively; the radial alignment and elongation of the ellipses indicate

the myocardial wall thickening during systole. In diastole, the circumferential alignment of the ellipses documents the corresponding wall thinning.

Comparison with tissue Doppler

Agreement between Multiscale Motion Mapping and tissue Doppler velocities was assessed in 132 separate measurements in the center of each segment from 11 clinical echocardiograms for which B-mode and tissue Doppler signals had been acquired simultaneously. For comparison, only the motion vector component parallel to the ultrasound beam directions was used from Multiscale Motion Mapping because tissue Doppler is unable to measure the motion component perpendicular to the beam. There was a good correlation between Multiscale Motion Mapping and Doppler, with a correlation coefficient of 0.94 ($p<0.001$; regression line: $y = 0.87x - 0.14$). Bland-Altman analysis showed no significant bias (mean velocity difference: 0.223 cm/s, p=NS, SD=1.527 cm/s (7.2% of measured range)).

Clinical validation

Clinical applicability is a major requirement for a new technology. We collected prospectively a consecutive series of clinical echocardiograms from 125 hospitalized patients (mean age 64 ± 14 years, 33% judged as normal by conventional diagnosis) referred for echocardiography for clinical indications. Image quality was deemed sufficient for quantification in 114 cases (91.2%). Multiscale motion analysis was applied independently by two blinded users and produced completely reproducible motion maps. For each data set, segmental motion measures were extracted by the two users who specified subjectively locations in the center of each segment. Interobserver variability of velocity measurements (SD) was 0.896 cm/s (5.1% of measured range)), with a mean velocity difference of -0.077 cm/s (p=0.04) and a correlation coefficient between the two observers of 0.83 ($p<0.001$). The intraobserver variability of velocity measurements (SD) was 0.568 cm/s (3.2% of measured range) with a mean velocity difference of -0.063 cm/s (p=NS). The corresponding correlation coefficient was 0.93 ($p<0.001$).

Automatic objective classification of the measured velocities by the artificial neural network led to the global, binary classification as normal or abnormal contractility. Objective classification corresponded to the "majority vote" of subjective expert

rating in 84% of cases. Interobserver agreement of subjective reading (kappa=0.617) was only moderate. Interobserver agreement for classification based on Multiscale Motion Mapping was good (kappa=0.740).

Comprehensive objective motion analysis: Case study

To exemplify the practical application of Multiscale Motion Mapping, an example of a routine echocardiogram, for which local echo experts disagreed as to the presence or absence of motion abnormalities, is given in Figure 6. Figure 6(a) and (b) show the native grayscale loop together with 2D motion arrows in the septum and the lateral wall during systole and diastole, respectively. They show that there is paradoxical motion of the basal interventricular septum. Additional insight can be gained through separate display of transverse ('towards the centerline') and longitudinal ('along the centerline') ventricular motion in the same loop as shown in Figure 6(c) and (d), respectively. The motion components at mid-systole indicate that there is reduced longitudinal velocities of the basal left ventricle (p<0.01 vs normal) while transverse velocity of the lateral segments was in the normal range, and transverse velocity was negative in the basal septum. 2D strain rate, however, was normal (peak systolic thickening/thinning strain rates in the basal septum: 1.28 s^{-1} and -1.03 s^{-1}; p=NS vs normal, with maximum thickening directed towards the mid-ventricle, and a corresponding behavior in diastole).

These findings of objective, quantitative analysis—namely, paradoxical motion but normal thickening of the septum, combined with impaired long-axis but normal transverse function of the lateral segment—agree nicely with careful subjective analysis of the echocardiogram. Such comprehensive, objective evaluation of heart motion is not possible with any other echocardiographic technique.

Discussion

This is the first clinical description of Multiscale Motion Mapping, a novel computer vision-based approach for quantification of motion in echocardiograms. Based on comprehensive mathematical analysis of digital images, and using strategies similar in several aspects to the human visual system, Multiscale Motion Mapping allows visualization and quantification of true 2D heart motion independent from borders, Doppler and beam angles. From a single conventional grayscale dataset, Multiscale

Motion Mapping is able to quantify absolute local velocity, 2D velocity direction, 2D strain rates and principal axes of strain components.

The ability to objectively quantify heart function is much needed today for a number of reasons: the epidemic of heart failure calls for improved methods to diagnose impaired myocardial function at an early stage, to follow its course quantitatively and to study the impact of new therapeutic strategies in a noninvasive, but objective manner. The ever-increasing population segment in the western world that is at risk for ischemic heart disease renders noninvasive diagnostic methods like stress echocardiography more and more important, but also exposes their Achilles heel; namely, subjectivity and limited interobserver agreement. Last but not least, noninvasive examinations may lead to invasive procedures; further improvements in the objectivity of echo may thus also influence cost efficiency in cardiology.

While the reliability in the description of anatomy, of intracardiac flows and of valve function have reached a high level in the forty years since echocardiography was invented, determination of myocardial function has lagged behind for several reasons: First, cardiac motion is very complex: even at a single location, it consists of components that may either be independent from each other, such as passive heart translation and active myocardial thickening, or that are physiologically connected like shortening along the myocardial fiber axis and thickening perpendicular to the fiber axis. Too simple motion models may thus be insufficient to describe such motion correctly.

Second, in conventional 2D echocardiograms studied here, our visual system is able to detect full 2D motion patterns while conventional analysis methods are typically one-dimensional: border detection algorithms detect motion perpendicular to the endocardium; tissue Doppler detects motion parallel to the ultrasound beam. (Clearly, out-of-plane motion also exists in echo; this is probably best examined in dynamic 3D imaging; although not a topic of this manuscript, it is in principle also accessible to the described approach). The key weakness of 1D methods is well-known for conventional Doppler where motion near 90 degree to the beam cannot be detected, but it is less well-known that this poses a particular problem for Doppler-based deformation imaging, as geometry predicts that there are two "blind spots" for Doppler deformation imaging of myocardial contraction near 45 and 135 degrees.

An important determinant of actual use of new technology in echocardiography is the ease of performing and interpreting measurements. Here, Multiscale Motion Mapping offers two new aspects: In the color display, velocities can be encoded such that e.g. inward motion takes the same color in multiple segments (Figure 5(c), (d)), an evident simplification compared to tissue Doppler, where Doppler angle dependency leads to a multitude of colors even though the same absolute velocity actually may be present. In the arrow display, simple mouse clicks allow determination, visualization and quantitative export in a spreadsheet of both, motion direction and absolute value. Multiscale Motion Mapping thus extends current technology, by making available more detailed quantitative motion information compared to either visual analysis, Doppler velocity imaging, Doppler deformation imaging, or border detection strategies like Color Kinesis[14], while readability is maintained.

Current limitations of Multiscale Motion Mapping include limited availability of the method on commercial machines, a point easily addressable since no hardware changes are needed to implement the method on a digital echo machine (currently, it is implemented on an external analysis package). As for the human eye, there is a limit of image quality, below which recognition and measurement of structures and motion becomes infeasible. In our consecutive series of clinical echocardiograms, this was a problem in < 10% of cases; this robustness probably originates in the exploitation of spatial and temporal coherence (see in methods section); nevertheless, we expect that the ongoing echo hardware evolution will further improve the applicability of computer vision approaches in echocardiography. As this is a beat-to-beat analysis, the pitfall of measuring non-representative beats in arrhythmia, but also the potential to compare beat-to-beat variability of contraction need to be addressed. Clearly, this first clinical description needs to be followed by more thorough clinical validation and application in a wide variety of clinical problems. Clinical studies applying Multiscale Motion Mapping to routine echo, heart failure quantification, and stress echo are ongoing at present.

We believe that Multiscale Motion Mapping may have a significant impact on the practice of echocardiography: first, it allows exploration of complex features of heart motion inaccessible to current echocardiographic techniques, such as quantitative

assessment of apical twisting motion, as well as direct comparison of axial shortening, radial motion, and local thickening of the myocardium.

Second, it expands the toolbox of the cardiologist by a quantitative tool that could be profitably applied in routine echocardiography for improved definition of normal versus abnormal LV function (probably the most frequent indication for echo); likewise, improved quantitative analysis may overcome limitations of echocardiography in diagnosis and longitudinal assessment of heart failure, and may reduce the interobserver variability of stress echocardiography. As determination of global ventricular function (by integration of regional motility), and evaluation of asynchrony of contraction (by comparing time course of velocities) is done at the same time, application of the method to patients with bundle branch block and resynchronization therapy appears also promising.

This first clinical report of Multiscale Motion Mapping thus opens a new door for improved analysis of cardiac motion. Availability of full 2D information of both, displacement and deformation, unaffected by the known limitations of Doppler, allows not only exploration of the complex features of cardiac motion inaccessible to current techniques, but appears also useful to render a wide range of clinical echocardiography more objective and quantitative.

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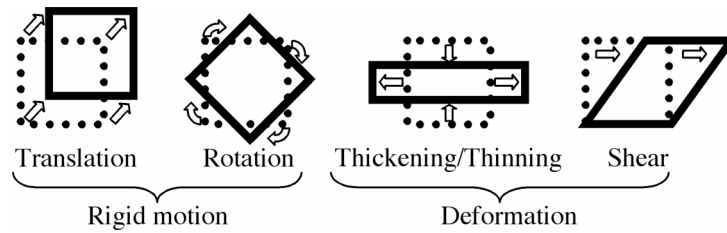
Figure 1: *Typical motion patterns of the heart that can be described by an affine motion model.*
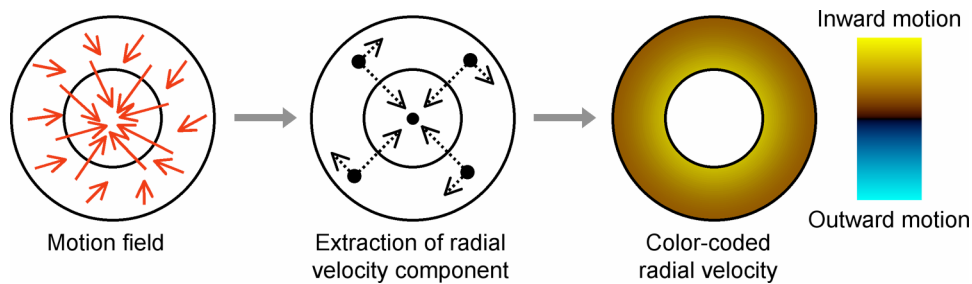

a) *Visualization of estimated velocities*
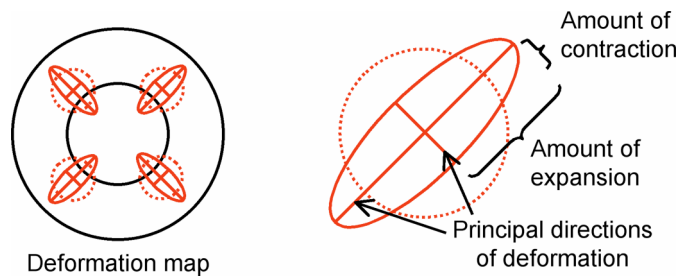
b) *Visualization of 2D deformation by means of ellipses*

Figure 2: *Capabilities of "Triple-M"-imaging to extract and visualize different aspects of motion. The estimated motion is represented as a motion field (a)(left). The radial motion component towards a reference point can be extracted and visualized in color-coded form (a)(right). Regional deformation magnitudes and directions are represented in the form of ellipses (b).*
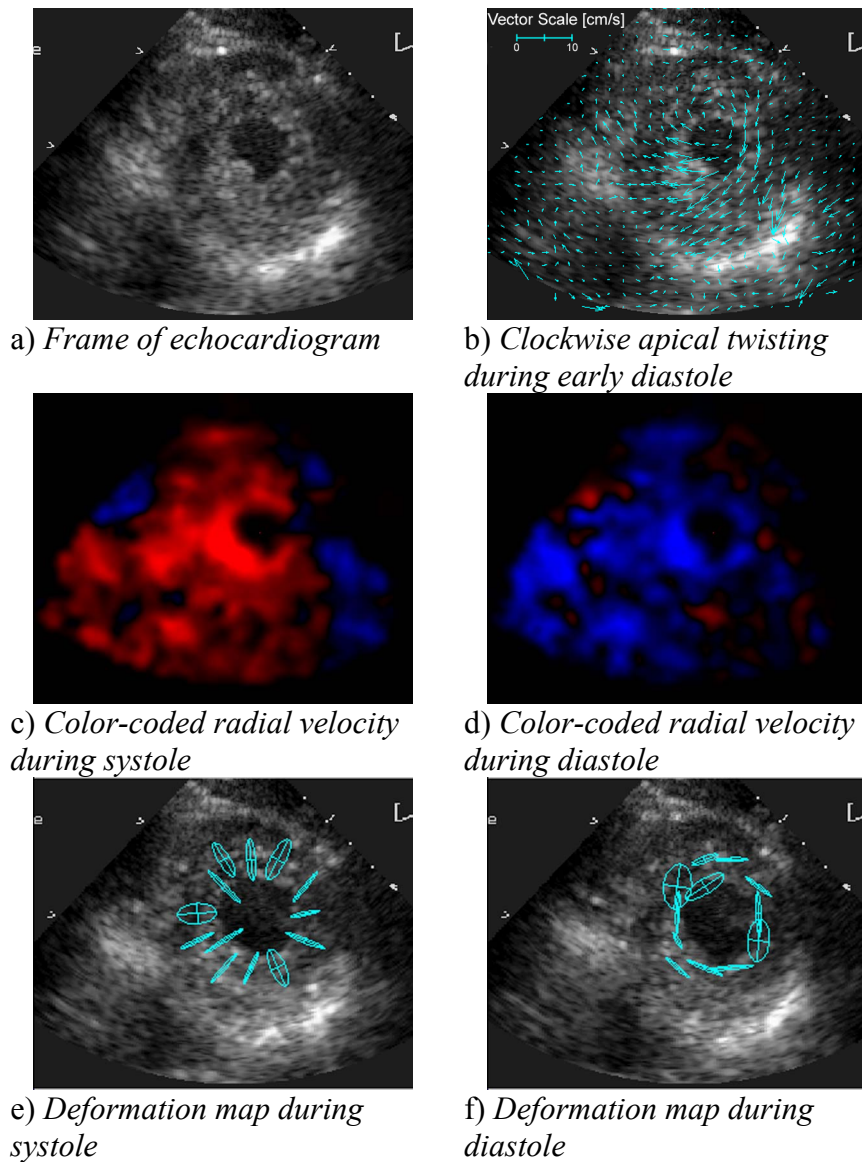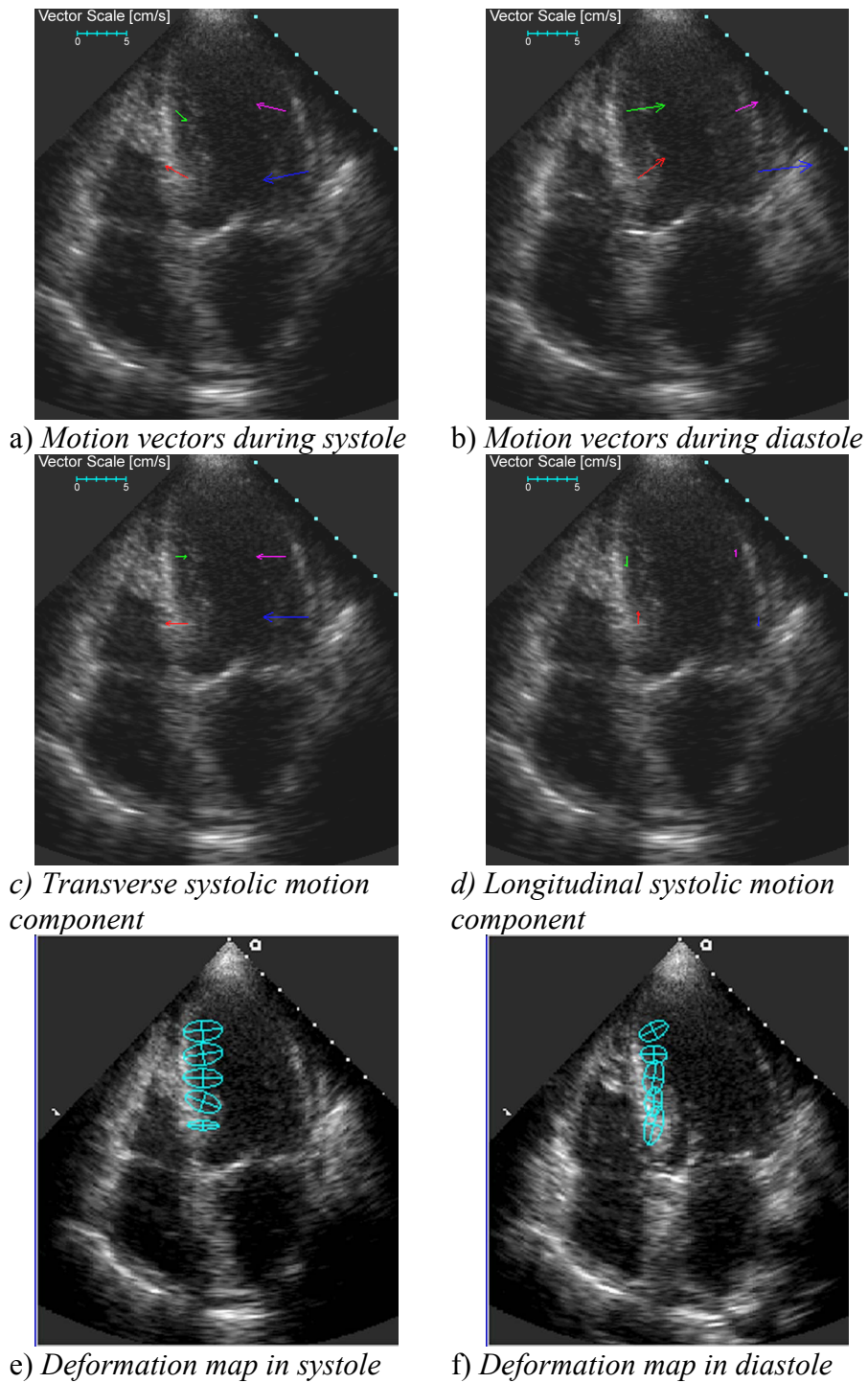
a) *Synthetic echo loop*   b) *Velocity field*

c) *Radial velocity*   d) *Strain rate*
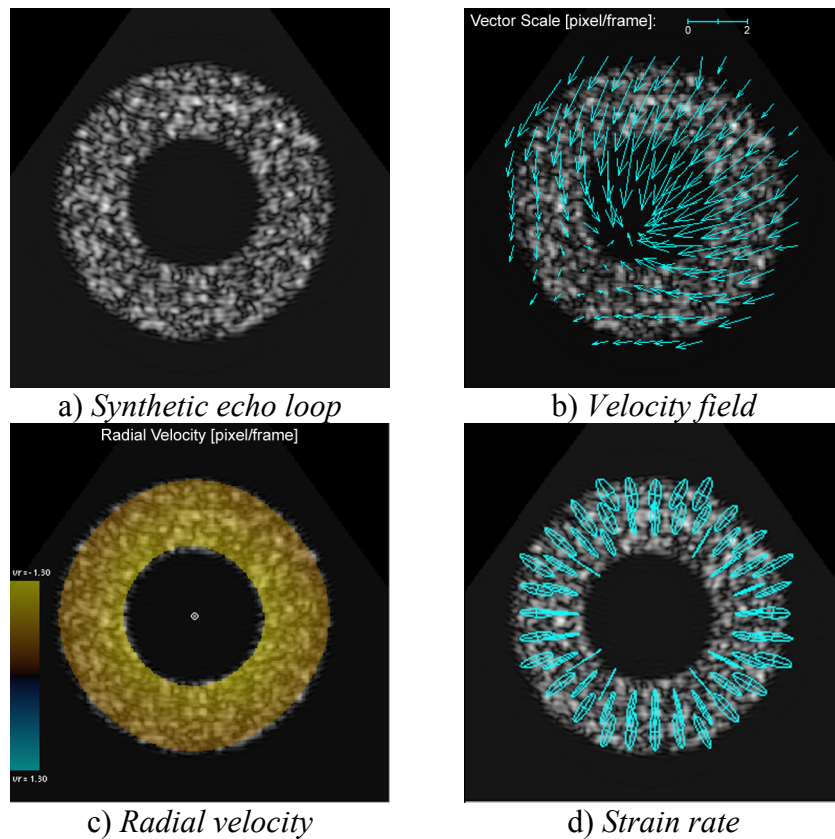
Figure 3: *Different kinds of motion information determined by Multiscale Motion Mapping from synthetic ultrasound data (a) during systole: the velocity display (b) reflects the superposition of radial contraction and global translation. The radial velocity component (c) indicates uniform inward motion (a reference point moving with the cavity was used here). The strain rate display (d) documents myocardial thickening and circumferential shortening independently from the underlying translation.*

a) *Frame of B-mode echo* b) *Motion in Multiscale Motion Mapping* c) *Color Doppler signal*
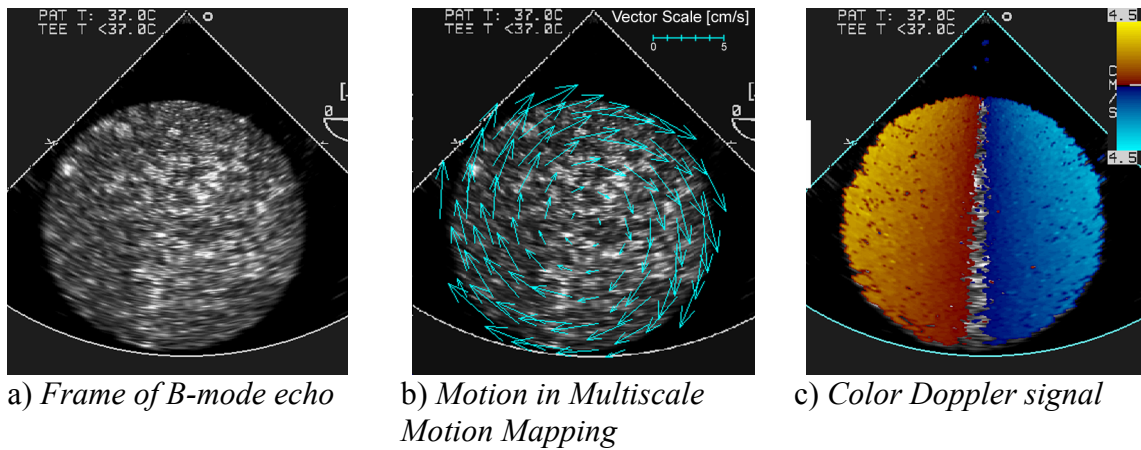
Figure 4: *Rotating phantom experiment. (a) original echo loop, (b) motion field by Multiscale Motion Mapping reflecting rotational motion. For comparison, the tissue Doppler signal is displayed in (c): despite identical angular velocity at all points on a given concentric circle, color encoding changes continuously due to the angle dependency of Doppler, in contrast to the arrow display of Multiscale Motion Mapping.*

a) *Frame of echocardiogram*

b) *Clockwise apical twisting during early diastole*

c) *Color-coded radial velocity during systole*

d) *Color-coded radial velocity during diastole*

e) *Deformation map during systole*

f) *Deformation map during diastole*

Figure 5: *Multiscale Motion Mapping in an apical short axis view of a normal heart. Clockwise apical twisting during diastole is documented by the motion arrows in (b). Radial inward (c) and outward motion (d) during systole and diastole displayed as red and blue color map (here using a fixed reference point in the center). Myocardial radial wall thickening and circumferential shortening during systole is indicated by the deformation map (e). The reversed deformation during diastole is presented in (f).*

a) *Motion vectors during systole*   b) *Motion vectors during diastole*

c) *Transverse systolic motion component*   d) *Longitudinal systolic motion component*

e) *Deformation map in systole*   f) *Deformation map in diastole*

Figure 6: *Case study in apical four-chamber view. Multiscale Motion mapping indicates paradoxical motion of the interventricular septum (outward during systole (a), inward during diastole (b)). Separate analysis of transverse (c) and longitudinal motion (d) shows impaired longitudinal velocities but normal transverse velocities (lateral wall) during systole. Despite the paradoxical septal velocities, deformation imaging shows normal radial thickening with shortening along the septum during systole (e), documenting normal contractility of the septum, with reciprocal findings in diastole (f).*