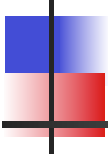
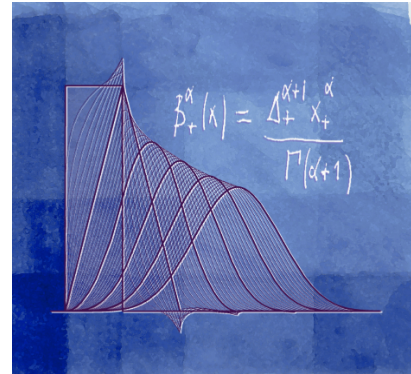


## Sparse stochastic processes: A statistical framework for compressed sensing and biomedical image reconstruction



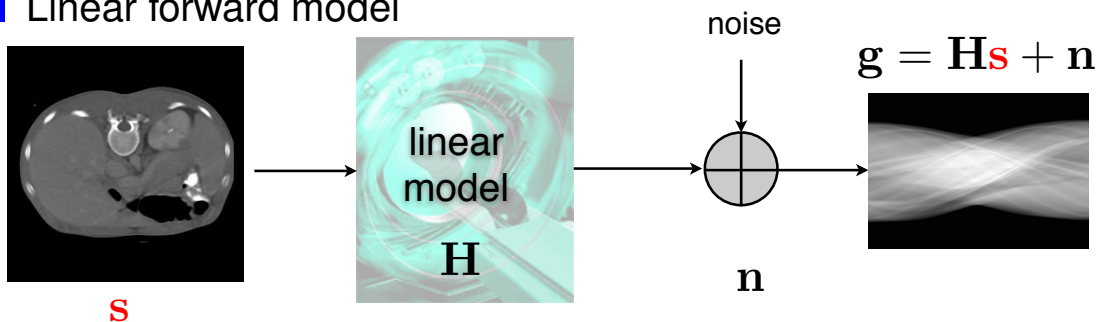
Michael Unser  
Biomedical Imaging Group  
EPFL, Lausanne, Switzerland



Tutorial, Inverse Problems and Imaging Conference, Institut Henri Poincaré, Paris, April 7-11, 2014.

## Variational formulation of image reconstruction

### Linear forward model



Ill-posed inverse problem: recover  $\mathbf{s}$  from noisy measurements  $\mathbf{g}$

### Reconstruction as an optimization problem

$$\mathbf{s}^* = \operatorname{argmin} \underbrace{\|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2}_{\text{data consistency}} + \underbrace{\lambda \mathcal{R}(\mathbf{s})}_{\text{regularization}}$$

## Classical linear reconstruction

$$\mathbf{s}^* = \underset{\mathbf{s}}{\operatorname{argmin}} \underbrace{\|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2}_{\text{data consistency}} + \underbrace{\lambda\mathcal{R}(\mathbf{s})}_{\text{regularization}}$$

- Quadratic regularization (Tikhonov)

$$\mathcal{R}(\mathbf{s}) = \|\mathbf{L}\mathbf{s}\|^2$$

$$\text{Formal linear solution: } \mathbf{s} = (\mathbf{H}^T\mathbf{H} + \lambda\mathbf{L}^T\mathbf{L})^{-1}\mathbf{H}^T\mathbf{g} = \mathbf{R}_\lambda \cdot \mathbf{g}$$

$$\Updownarrow \quad \mathbf{L} = \mathbf{C}_s^{-1/2}: \text{Whitening filter}$$

- Statistical formulation under Gaussian hypothesis

Wiener (LMMSE) solution = Gauss MMSE = Gauss MAP

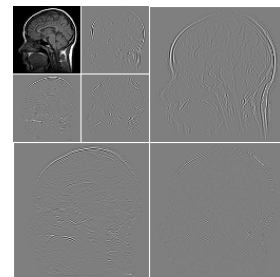
$$\mathbf{s}_{\text{MAP}} = \underset{\mathbf{s}}{\operatorname{argmin}} \underbrace{\frac{1}{\sigma^2}\|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2}_{\text{Data Log likelihood}} + \underbrace{\|\mathbf{C}_s^{-1/2}\mathbf{s}\|_2^2}_{\text{Gaussian prior likelihood}}$$

$$\text{Signal covariance: } \mathbf{C}_s = \mathbb{E}\{\mathbf{s} \cdot \mathbf{s}^T\}$$

3

## Sparsity-promoting reconstruction algorithms

$$\mathbf{s}^* = \underset{\mathbf{s}}{\operatorname{argmin}} \underbrace{\|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2}_{\text{data consistency}} + \underbrace{\lambda\mathcal{R}(\mathbf{s})}_{\text{regularization}}$$



- Wavelet-domain regularization

Wavelet expansion:  $\mathbf{s} = \mathbf{W}\mathbf{v}$  (typically, sparse)

Wavelet-domain sparsity-constraint:  $\mathcal{R}(\mathbf{s}) = \|\mathbf{v}\|_{\ell_1}$  with  $\mathbf{v} = \mathbf{W}^{-1}\mathbf{s}$

Iterated shrinkage-thresholding algorithm (ISTA, FISTA, FWISTA)

- $\ell_1$  regularization (Total variation)

$\mathcal{R}(\mathbf{s}) = \|\mathbf{L}\mathbf{s}\|_{\ell_1}$  with  $\mathbf{L}$ : gradient

Iterative reweighted least squares (IRLS) or FISTA

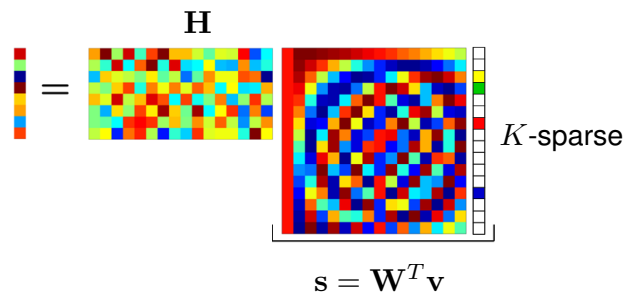
4

# Theory of compressive sensing

## ■ Generalized sampling setting (after discretization)

■ Linear inverse problem:  $\mathbf{u} = \mathbf{H}\mathbf{s} + \mathbf{n}$

■  $N_u \times N_v$  system matrix:  $\mathbf{A} = \mathbf{H}\mathbf{W}^T$



## ■ Formulation of ill-posed recovery problem when $2K < N_u \ll N_v$

$$(P0) \min_{\mathbf{v}} \|\mathbf{u} - \mathbf{A}\mathbf{v}\|_2^2 \quad \text{subject to} \quad \|\mathbf{v}\|_0 \leq K$$

## ■ Theoretical result

Under suitable conditions on  $\mathbf{A}$  (e.g., restricted isometry), the solution is unique and the recovery problem (P0) is equivalent to:

$$(P1) \min_{\mathbf{v}} \|\mathbf{u} - \mathbf{A}\mathbf{v}\|_2^2 \quad \text{subject to} \quad \|\mathbf{v}\|_1 \leq C_1$$

[Donoho et al., 2005  
Candès-Tao, 2006, ...]

## Key research questions

### ① Discretization of reconstruction problem

*Continuous-domain formulation*

**Generalized sampling**

### ② Formulation of ill-posed reconstruction problem

*Statistical modeling (beyond Gaussian)  
supporting non-linear reconstruction schemes  
(including CS)*

**Sparse stochastic processes**

### ③ Efficient implementation for large-scale imaging problem

**FISTA, ADMM**

# OUTLINE

---

- Variational formulation of inverse problems ✓
- **Part I: Statistical modeling**  
An introduction to sparse stochastic processes
  - Generalized innovation model
  - Statistical characterization of signal
- **Part II: Recovery of sparse signals**  
Reconstruction of biomedical images
  - Discretization of inverse problem
  - Generic MAP estimator (iterative reconstruction algorithm)
  - Applications



*Deconvolution microscopy*  
*Magnetic resonance imaging*  
*X-ray tomography*  
*Phase-contrast tomography*

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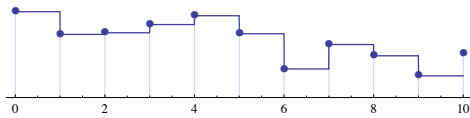
An abstract graphic consisting of a grid of squares in various shades of blue, teal, and green, creating a textured, pixelated effect. The text is overlaid on this background.

An  
introduction  
to sparse  
stochastic  
processes

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# Splines and Legos revisited

- Cardinal spline of degree 0: piecewise-constant



$$f_1(t) = \sum_{k \in \mathbb{Z}} f_1[k] \beta_+^0(t - k)$$

$$\beta_+^0(t) = \begin{cases} 1, & \text{for } 0 \leq t < 1 \\ 0, & \text{otherwise.} \end{cases}$$

Notion of D-spline:

$$Df_1(t) = \sum_{k \in \mathbb{Z}} a_1[k] \delta(t - k)$$

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## B-spline and derivative operator

Derivative  $Df(t) = \frac{df(t)}{dt}$        $D \xleftrightarrow{\mathcal{F}} j\omega$

Finite difference operator

$$D_d f(t) = f(t) - f(t - 1) \qquad D_d \xleftrightarrow{\mathcal{F}} 1 - e^{-j\omega}$$

$$= (\beta_+^0 * Df)(t)$$

B-spline of degree 0

$$\beta_+^0(t) = D_d D^{-1} \delta(t) = D_d \mathbb{1}_+(t)$$

$\Downarrow$

$$\hat{\beta}_+^0(\omega) = \frac{1 - e^{-j\omega}}{j\omega}$$

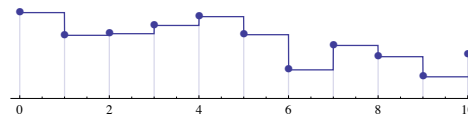
$$\beta_+^0(t) = \mathbb{1}_+(t) - \mathbb{1}_+(t - 1)$$



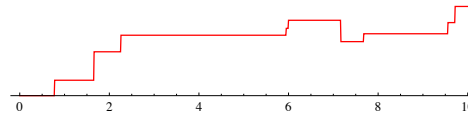
10

# Random spline: archetype of sparse signal

cardinal



non-uniform



$$Ds(t) = \sum_n a_n \delta(t - t_n) = w(t)$$

Random weights  $\{a_n\}$  i.i.d. and random knots  $\{t_n\}$  (Poisson with rate  $\lambda$ )

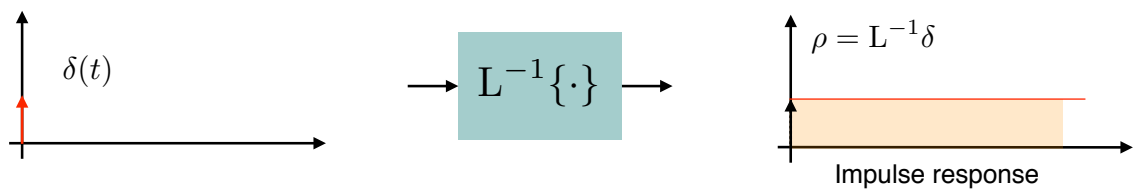
## ■ Anti-derivative operators

Shift-invariant solution:  $D^{-1}\varphi(t) = (\mathbb{1}_+ * \varphi)(t) = \int_{-\infty}^t \varphi(\tau) d\tau$

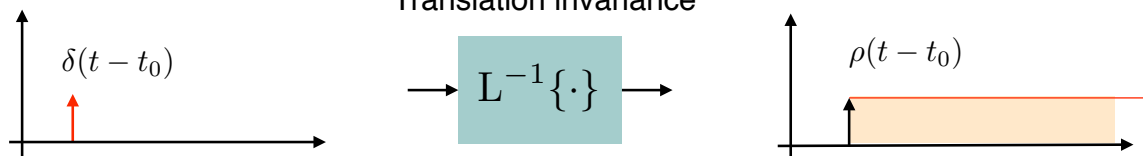
Scale-invariant solution:  $D_0^{-1}\varphi(t) = \int_0^t \varphi(\tau) d\tau$

# Innovation-based synthesis

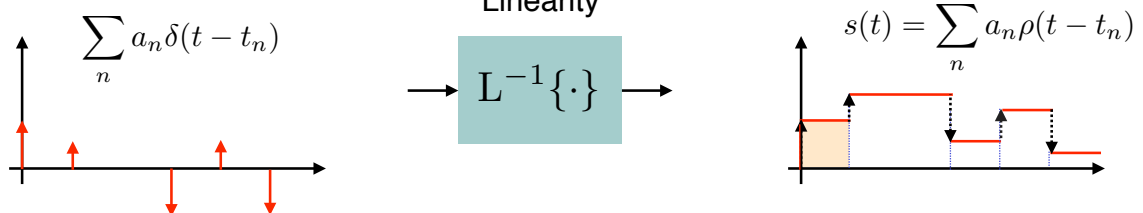
$$L = \frac{d}{dt} = D \Rightarrow L^{-1}: \text{integrator}$$



Translation invariance



Linearity

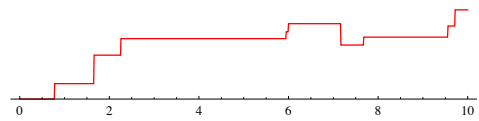


# Compound Poisson process

## ■ Stochastic differential equation

$$Ds(t) = w(t)$$

with boundary condition  $s(0) = 0$



$$\text{Innovation: } w(t) = \sum_n a_n \delta(t - t_n)$$

## ■ Formal solution

$$\begin{aligned} s(t) &= D_0^{-1}w(t) = \sum_n a_n D_0^{-1}\{\delta(\cdot - t_n)\}(t) \\ &= \sum_n a_n (\mathbb{1}_+(t - t_n) - \mathbb{1}_+(-t_n)) \end{aligned}$$

(impose boundary condition)

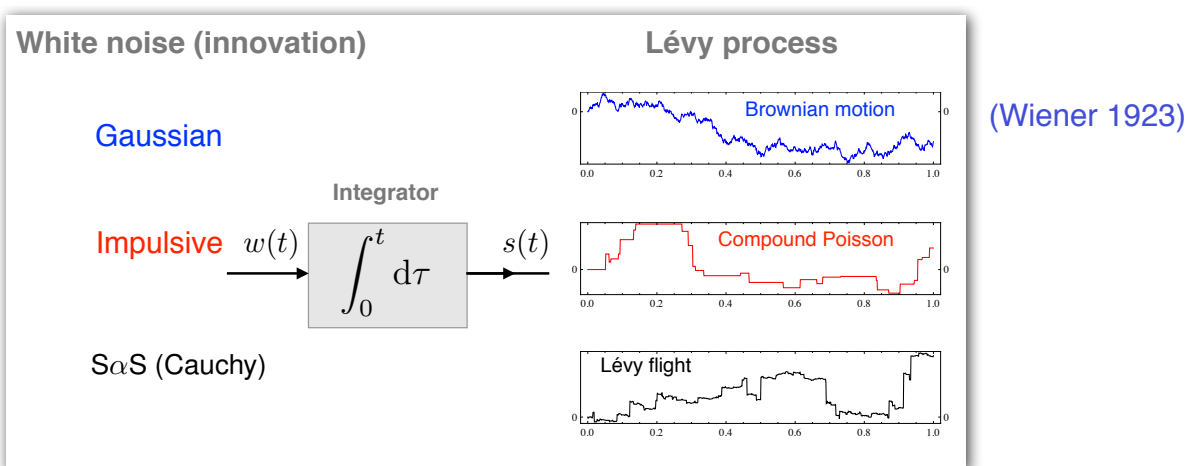
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# Lévy processes: all admissible brands of innovations

Generalized innovations : white Lévy noise with  $\mathbb{E}\{w(t)w(t')\} = \sigma_w^2 \delta(t - t')$

$$Ds = w \quad (\text{unstable SDE !})$$

$$s = D_0^{-1}w \quad \Leftrightarrow \quad \forall \varphi \in \mathcal{S}, \quad \langle \varphi, s \rangle = \langle D_0^{-1*} \varphi, w \rangle$$



(Paul Lévy circa 1930)

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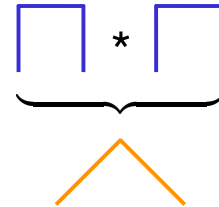
# Decoupling Lévy processes: increments

Increment process:  $u(t) = D_d s(t) = D_d D_0^{-1} w(t) = (\beta_+^0 * w)(t)$ .

Increment process is stationary with autocorrelation function

$$R_u(\tau) = \mathbb{E}\{u(t + \tau)u(t)\} = (\beta_+^0 * (\beta_+^0)^\vee * R_w)(\tau)$$

$$= \sigma_w^2 \beta_+^1(\tau - 1)$$



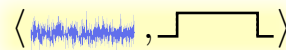
with  $(\beta_+^0)^\vee(t) = \beta_+^0(-t)$

## Discrete increments

$$u[k] = s(k) - s(k - 1) = \langle w, \mathbb{1}_{[k, k+1)} \rangle = \langle w, (\beta_+^0)^\vee(\cdot - k) \rangle.$$

$u[k]$  are i.i.d. because

- $\{(\beta_+^0)^\vee(\cdot - k)\}$  are non-overlapping
- $w$  is independent at every point (white noise)



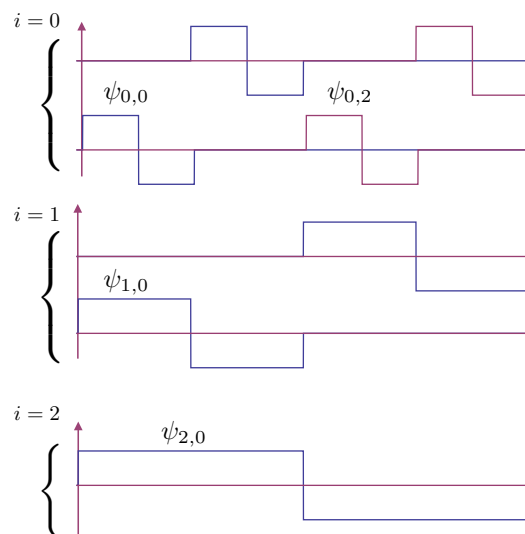
15

# Wavelet analysis of Lévy processes

## ■ Haar wavelets

$$\psi_{\text{Haar}}(t) = \begin{cases} 1, & \text{for } 0 \leq t < \frac{1}{2} \\ -1, & \text{for } \frac{1}{2} \leq t < 1 \\ 0, & \text{otherwise.} \end{cases}$$

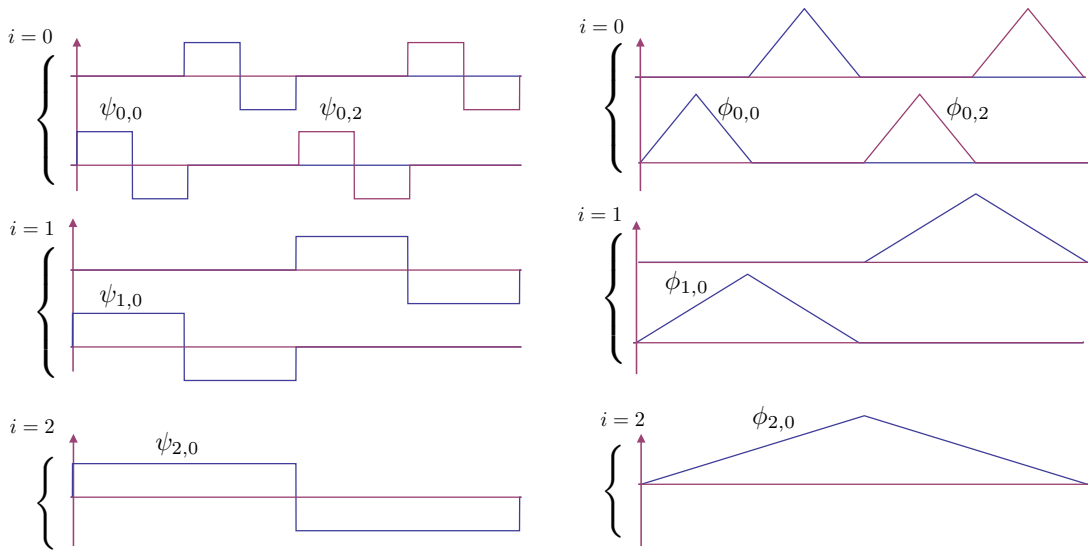
$$\psi_{i,k}(t) = 2^{-i/2} \psi_{\text{Haar}}\left(\frac{t - 2^i k}{2^i}\right)$$



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# Wavelets as multi-scale derivatives



## ■ Wavelet coefficients of Lévy process

$$\psi_{i,k} = 2^{i/2-1} D\phi_{i,k}$$

$$D_0^{-1}\psi_{i,k} = 2^{i/2-1}\phi_{i,k}$$

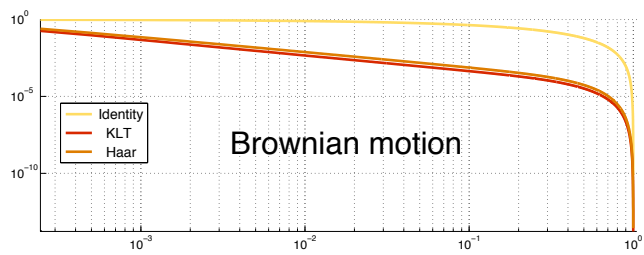
$$Y_{i,k} = \langle s, \psi_{i,k} \rangle \propto \langle s, D\phi_{i,k} \rangle$$

$$\propto \langle D^* s, \phi_{i,k} \rangle = -\langle w, \phi_{i,k} \rangle$$

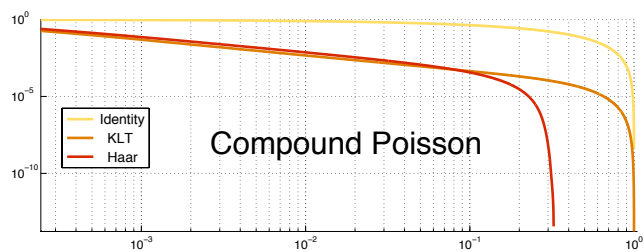
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# M-term approximation: wavelets vs. KLT

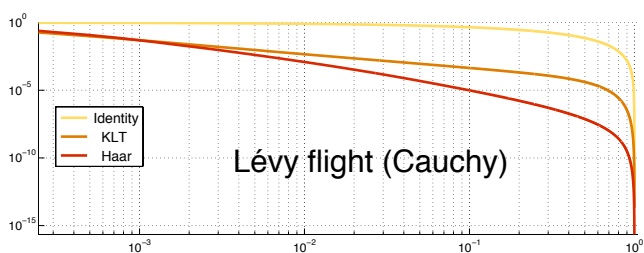
Gaussian



Finite rate of innovation



Even sparser ...

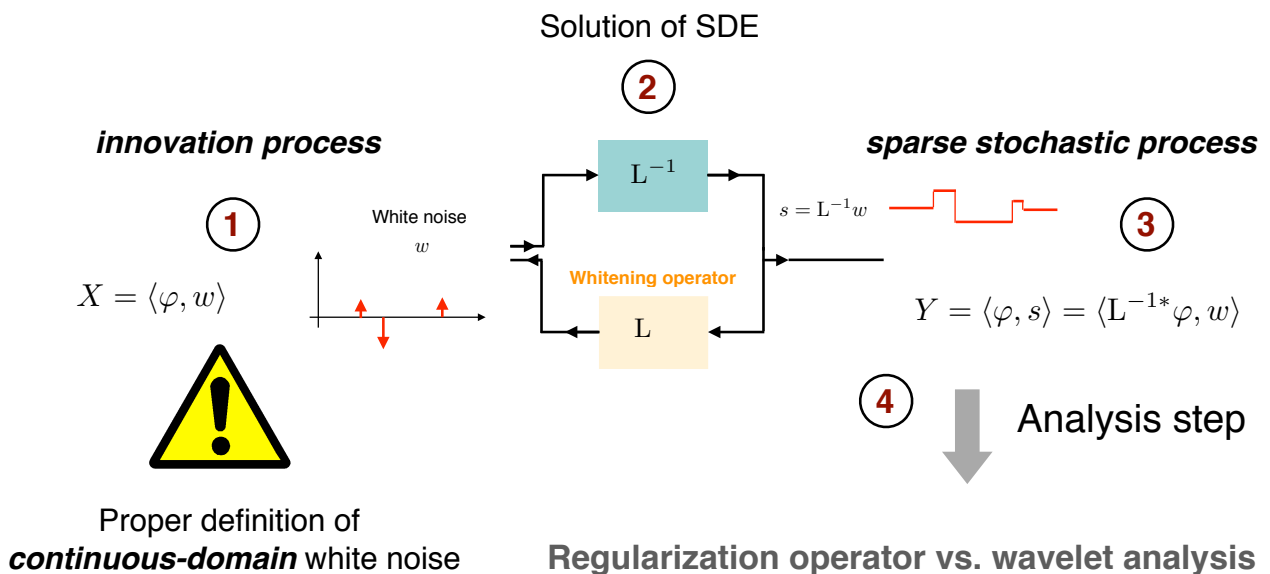


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# Generalized innovation model

Theoretical framework: Gelfand's theory of generalized stochastic processes

Generic test function  $\varphi \in \mathcal{S}$  plays the role of index variable



(Unser et al, IEEE-IT 2014)

# Short primer on probability theory

Random variable  $X$

## Probability measure and density function (pdf)

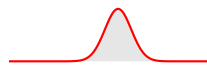
$$\text{Prob}(X \in E) = \mathcal{P}_X(E) = \int_E p_X(x) dx$$

$$\text{Expectation: } \mathbb{E}\{f(X)\} = \int_{\mathbb{R}} f(x) \mathcal{P}_X(dx) = \int_{\mathbb{R}} f(x) p_X(x) dx$$

## Characteristic function

$$\hat{p}_X(\omega) = \mathbb{E}\{e^{j\omega X}\} = \int_{\mathbb{R}} e^{j\omega x} p_X(x) dx$$

### Example: Gaussian



$$p_X(x) = \frac{1}{\sqrt{2\pi}} e^{-x^2/2}$$

$$\updownarrow \mathcal{F}$$

$$\hat{p}_X(\omega) = e^{-\omega^2/2}$$

### Bochner's theorem

Let  $\hat{p}_X : \mathbb{R} \rightarrow \mathbb{C}$  be a continuous, positive-definite function such that  $\hat{p}_X(0) = 1$ .

Then, there exists a unique Borel probability measure  $\mathcal{P}_X$  on  $\mathbb{R}$ , such that

$$\hat{p}_X(\omega) = \int_{\mathbb{R}} e^{j\omega x} \mathcal{P}_X(dx) = \int_{\mathbb{R}} e^{j\omega x} p_X(x) dx$$

# Generalized innovation process

■ Difficulty 1:  $w \neq w(x)$  is too rough to have a pointwise interpretation



■ Difficulty 2:  $w$  is an infinite-dimensional random entity;  
its “pdf” can be formally specified by a measure  $\mathcal{P}_w(E)$  where  $E \subseteq \mathcal{S}'(\mathbb{R}^d)$

■ Axiomatic definition

(Gelfand-Vilenkin 1964)

$w$  is a generalized innovation process (or continuous-domain white noise) in  $\mathcal{S}'(\mathbb{R}^d)$  if

1. **Observability** :  $X = \langle \varphi, w \rangle$  is a well-defined random variable for any test function  $\varphi \in \mathcal{S}(\mathbb{R}^d)$ .
2. **Stationarity** :  $X_{x_0} = \langle \varphi(\cdot - x_0), w \rangle$  is identically distributed for all  $x_0 \in \mathbb{R}^d$ .
3. **Independent atoms** :  $X_1 = \langle \varphi_1, w \rangle$  and  $X_2 = \langle \varphi_2, w \rangle$  are independent whenever  $\varphi_1$  and  $\varphi_2$  have non-intersecting support.

$$X_1 = \langle \text{[blue noise]}, \text{[red pulse]} \rangle$$

$$X_2 = \langle \text{[blue noise]}, \text{[red pulse]} \rangle$$

■ Characteristic functional  $(\omega \rightarrow \varphi)$

$$\widehat{\mathcal{P}}_w(\varphi) = \mathbb{E}\{e^{j\langle \varphi, w \rangle}\} = \int_{\mathcal{S}'} e^{j\langle \varphi, g \rangle} \mathcal{P}_w(dg)$$

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finite-dimensional	infinite-dimensional
random variable $X$ in $\mathbb{R}^N$	generalized stochastic process $s$ in $\mathcal{S}'$
probability measure $\mathcal{P}_X$ on $\mathbb{R}^N$ $\mathcal{P}_X(E) = \text{Prob}(X \in E) = \int_E p_X(\mathbf{x}) \, d\mathbf{x}$ ( $p_X$ is a generalized [i.e., hybrid] pdf) for suitable subsets $E \subset \mathbb{R}^N$	probability measure $\mathcal{P}_s$ on $\mathcal{S}'$ $\mathcal{P}_s(E) = \text{Prob}(s \in E) = \int_E \mathcal{P}_s(dg)$ for suitable subsets $E \subset \mathcal{S}'$
characteristic function $\widehat{\mathcal{P}}_X(\omega) = \mathbb{E}\{e^{j\langle \omega, X \rangle}\} = \int_{\mathbb{R}^N} e^{j\langle \omega, \mathbf{x} \rangle} p_X(\mathbf{x}) \, d\mathbf{x}$ , $\omega \in \mathbb{R}^N$	characteristic functional $\widehat{\mathcal{P}}_s(\varphi) = \mathbb{E}\{e^{j\langle \varphi, s \rangle}\} = \int_{\mathcal{S}'} e^{j\langle \varphi, g \rangle} \mathcal{P}_s(dg)$ , $\varphi \in \mathcal{S}$

**Table 3.2** Comparison of notions of finite-dimensional statistical calculus with the theory of generalized stochastic processes. See Sections 3.4 for an explanation.

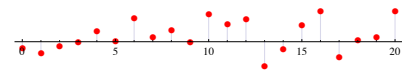
$\mathcal{S}$ : Schwartz' space of smooth (infinitely differentiable) and rapidly decaying functions

$\mathcal{S}'$ : Schwartz' space of tempered distributions (generalized functions)

# Defining Gaussian noise: discrete vs. continuous

Lévy exponent:  $\log \hat{p}_X(\omega) = f(\omega) = -\frac{1}{2}\omega^2$

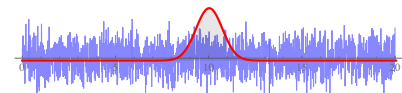
## Discrete white Gaussian noise



$X = (X_1, \dots, X_N)$  with  $X_n$  i.i.d standardized Gaussian

Characteristic function:  $\hat{p}_X(\omega) = \mathbb{E}\{e^{j\langle \omega, X \rangle}\} = \exp\left(\sum_{n=1}^N f(\omega_n)\right) = e^{-\frac{1}{2}\|\omega\|^2}$

## Continuous-domain white Gaussian noise



Infinite-dimensional entity  $w$  with generic observations  $X_n = \langle \varphi_n, w \rangle$

Characteristic functional:  $\widehat{\mathcal{P}}_w(\varphi) = \mathbb{E}\{e^{j\langle \varphi, w \rangle}\} = e^{-\frac{1}{2}\|\varphi\|_{L_2}^2} = \exp\left(\int_{\mathbb{R}} f(\varphi(x))dx\right)$

$\hat{p}_{X_n}(\omega) = \mathbb{E}\{e^{j\omega \langle \varphi_n, w \rangle}\} = \mathbb{E}\{e^{j\langle \omega \varphi_n, w \rangle}\} = \widehat{\mathcal{P}}_w(\omega \varphi_n) = e^{-\frac{1}{2}\omega^2 \|\varphi_n\|_{L_2}^2}$



# Infinite divisibility and Lévy exponents

**Definition:** A random variable  $X$  with generic pdf  $p_{id}(x)$  is **infinitely divisible** (id) iff., for any  $N \in \mathbb{Z}^+$ , there exist i.i.d. random variables  $X_1, \dots, X_N$  such that  $X \stackrel{d}{=} X_1 + \dots + X_N$ .

## Rectangular test function

$$\begin{aligned}
 X_{id} = \langle w, \text{rect} \rangle &= \langle \text{[noise]}, \text{[rect]} \rangle \\
 &= \langle \text{[noise]}, \text{[rect]} \rangle + \dots + \langle \text{[noise]}, \text{[rect]} \rangle
 \end{aligned}$$

### Proposition

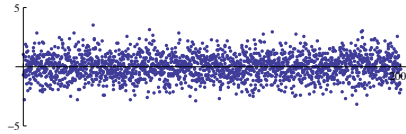
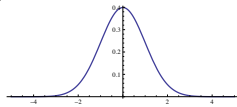
The random variable  $X_{id} = \langle w, \text{rect} \rangle$  where  $w$  is a generalized innovation process is infinitely divisible. It is uniquely characterized by its **Lévy exponent**  $f(\omega) = \log \hat{p}_{id}(\omega)$ .

**Bottom line:** There is a one-to-one correspondence between Lévy exponents and infinitely divisible distributions and, by extension, innovation processes.

# Examples of infinitely divisible laws

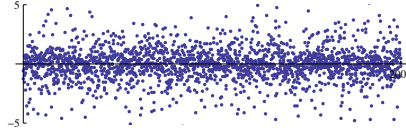
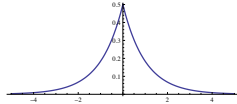
$$p_{id}(x)$$

(a) Gaussian



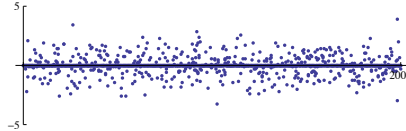
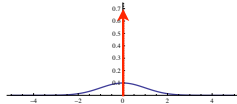
$$p_{\text{Gauss}}(x) = \frac{1}{\sqrt{2\pi\sigma^2}} e^{-\frac{x^2}{2\sigma^2}}$$

(b) Laplace



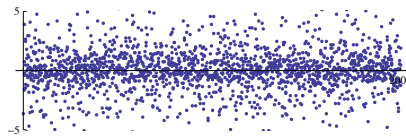
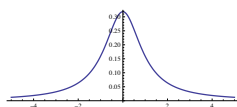
$$p_{\text{Laplace}}(x) = \frac{\lambda}{2} e^{-\lambda|x|}$$

(c) Compound Poisson



$$p_{\text{Poisson}}(x) = \mathcal{F}^{-1}\{e^{\lambda(\hat{p}_A(\omega)-1)}\}$$

(d) Cauchy (stable)



$$p_{\text{Cauchy}}(x) = \frac{1}{\pi(x^2 + 1)}$$

Sparser

$$\text{Characteristic function: } \hat{p}_{id}(\omega) = \int_{\mathbb{R}} p_{id}(x) e^{j\omega x} dx = e^{f(\omega)}$$

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# Characterization of generalized innovation

$$\begin{aligned} X_{\varphi} = \langle w, \varphi \rangle &= \langle \text{[stochastic process]}, \text{[smooth curve]} \rangle \triangleq \lim_{n \rightarrow \infty} \langle \text{[stochastic process]}, \text{[staircase]} \rangle \\ &= \lim_{n \rightarrow \infty} \langle \text{[stochastic process]}, \text{[rect]} \rangle + \dots + \langle \text{[stochastic process]}, \text{[rect]} \rangle \end{aligned}$$

## Theorem

Let  $w$  be a generalized stochastic process such that  $X_{id} = \langle w, \text{rect} \rangle$  is well-defined. Then,  $w$  is a generalized innovation (white noise) in  $\mathcal{S}'(\mathbb{R}^d)$  if and only if its characteristic form is given by

$$\widehat{\mathcal{P}}_w(\varphi) = \mathbb{E}\{e^{j\langle w, \varphi \rangle}\} = \exp\left(\int_{\mathbb{R}^d} f(\varphi(\mathbf{r})) d\mathbf{r}\right)$$

where  $f(\omega)$  is a **valid Lévy exponent** (in fact, the Lévy exponent of  $X_{id}$ ).

Moreover, the random variables  $X_{\varphi} = \langle w, \varphi \rangle$  are all **infinitely divisible** with modified Lévy exponent

$$f_{\varphi}(\omega) = \int_{\mathbb{R}^d} f(\omega\varphi(\mathbf{r})) d\mathbf{r}$$



# Canonical Lévy-Khintchine representation

## Definition

A (positive) measure  $\mu_v$  on  $\mathbb{R} \setminus \{0\}$  is called a **Lévy measure** if it satisfies

$$\int_{\mathbb{R}} \min(a^2, 1) \mu_v(da) = \int_{\mathbb{R}} \min(a^2, 1) v(a) da < \infty.$$

The corresponding **Lévy density**  $v : \mathbb{R} \rightarrow \mathbb{R}^+$  is such that  $\mu_v(da) = v(a)da$ .

## Theorem (Lévy-Khintchine)

A probability distribution  $p_{id}$  is **infinitely divisible** (id) iff. its characteristic function can be written as

$$\widehat{p}_{id}(\omega) = \int_{\mathbb{R}} p_{id}(x) e^{j\omega x} dx = \exp(f(\omega))$$

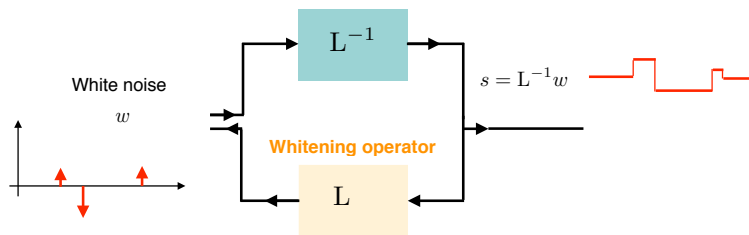
with

$$f(\omega) = \log \widehat{p}_{id}(\omega) = jb'_1\omega - \frac{b_2\omega^2}{2} + \int_{\mathbb{R} \setminus \{0\}} (e^{ja\omega} - 1 - ja\omega \mathbb{1}_{|a| < 1}(a)) v(a) da$$

where  $b'_1 \in \mathbb{R}$  and  $b_2 \in \mathbb{R}^+$  are some arbitrary constants, and where  $v$  is an admissible Lévy density. The function  $f$  is called the **Lévy exponent** of  $p_{id}$ .

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## Steps 2 + 3: Characterization of sparse process



### ■ Abstract formulation of innovation model

$$s = L^{-1}w \Leftrightarrow \forall \varphi \in \mathcal{S}, \quad \langle \varphi, s \rangle = \langle \varphi, L^{-1}w \rangle = \langle \underbrace{L^{-1*}\varphi}_w, w \rangle$$

$$\Rightarrow \widehat{\mathcal{P}}_s(\varphi) = \mathbb{E}\{e^{j\langle s, \varphi \rangle}\} = \widehat{\mathcal{P}}_w(L^{-1*}\varphi) = \exp\left(\int_{\mathbb{R}^d} f(L^{-1*}\varphi(\mathbf{x})) d\mathbf{x}\right)$$

Sufficient condition for existence:

$$L^{-1*} \text{ continuous operator: } \mathcal{S}(\mathbb{R}^d) \rightarrow L_p(\mathbb{R}^d)$$

(U.-Tafti-Sun, IEEE-IT 2014)

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# Innovation model: statistical implications (id)

- Statistical description of white Lévy noise  $w$  (innovation)

- Characterized by canonical ( $p$ -admissible) Lévy exponent  $f(\omega)$
- Generic observation:  $X = \langle \varphi, w \rangle$  with  $\varphi \in L_p(\mathbb{R}^d)$
- $X$  is **infinitely divisible** with (modified) Lévy exponent

$$f_\varphi(\omega) = \log \widehat{p}_X(\omega) = \int_{\mathbb{R}^d} f(\omega\varphi(x)) dx$$

- Linear observation of generalized stochastic process

$$s = L^{-1}w \Leftrightarrow \langle \psi, s \rangle = \langle \psi, L^{-1}w \rangle = \underbrace{\langle L^{-1*}\psi, w \rangle}$$

If  $\phi = L^{-1*}\psi \in L_p(\mathbb{R}^d)$  then  $Y = \langle \psi, s \rangle = \langle \phi, w \rangle$  is **infinitely divisible** with Lévy exponent  $f_\phi(\omega) = \int_{\mathbb{R}^d} f(\omega\phi(x)) dx$



$$\Rightarrow p_Y(y) = \mathcal{F}^{-1}\{e^{f_\phi(\omega)}\}(y) = \int_{\mathbb{R}} e^{f_\phi(\omega) - j\omega y} \frac{d\omega}{2\pi} = \text{explicit form of pdf}$$

## Example 1: (f)Brownian motion

$$Ds = w \quad (\text{unstable SDE !}) \quad D^\gamma s = w$$

$$s = D_0^{-1}w \Leftrightarrow \forall \varphi \in \mathcal{S}, \quad \langle \varphi, s \rangle = \langle D_0^{-1*}\varphi, w \rangle$$

$$L_2\text{-stable anti-derivative: } I_0^*\varphi(t) = \int_{\mathbb{R}} \frac{\widehat{\varphi}(\omega) - \widehat{\varphi}(0)}{-j\omega} e^{j\omega t} \frac{d\omega}{2\pi}$$

- Characteristic form of Brownian motion (a.k.a. Wiener process)

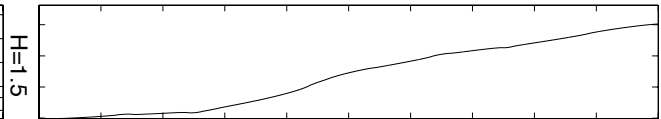
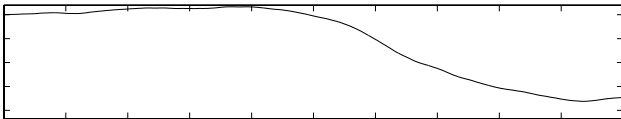
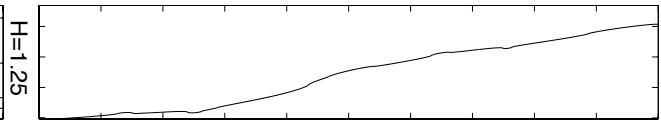
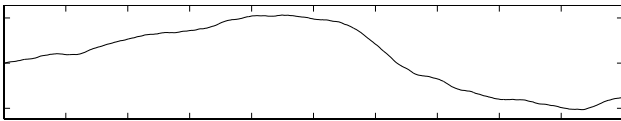
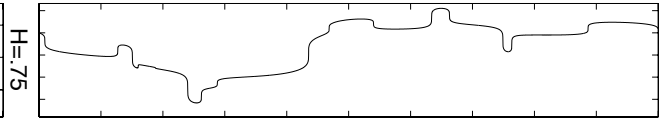
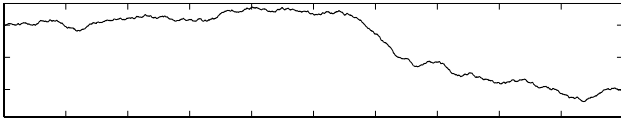
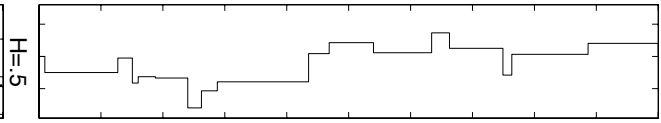
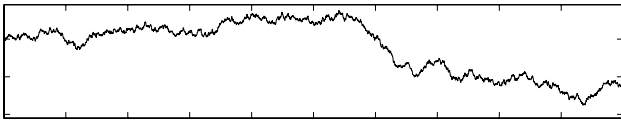
$$\begin{aligned} \widehat{\mathcal{P}}_W(\varphi) &= \exp\left(-\frac{1}{2}\|I_0^*\varphi\|_{L_2}^2\right) \\ &= \exp\left(-\frac{1}{2}\int_{\mathbb{R}} \left|\frac{\widehat{\varphi}(\omega) - \widehat{\varphi}(0)}{-j\omega}\right|^2 \frac{d\omega}{2\pi}\right) \end{aligned} \quad \begin{array}{l} \text{Stabilization} \Leftrightarrow \text{non-stationary behavior} \\ \text{(by Parseval)} \end{array}$$

- Characteristic form of fractional Brownian motion

$$\widehat{\mathcal{P}}_s(\varphi) = \exp\left(-\frac{1}{2}\int_{\mathbb{R}} \left|\frac{\widehat{\varphi}(\omega) - \widehat{\varphi}(0)}{|\omega|^\gamma}\right|^2 \frac{d\omega}{2\pi}\right) \quad (\text{Blu-U., IEEE-SP 2007})$$

## Example in 1D: Self-similar processes

$$L \xleftrightarrow{\mathcal{F}} (j\omega)^{H+\frac{1}{2}} \Rightarrow L^{-1}: \text{fractional integrator}$$



**Gaussian**

**Sparse (generalized Poisson)**

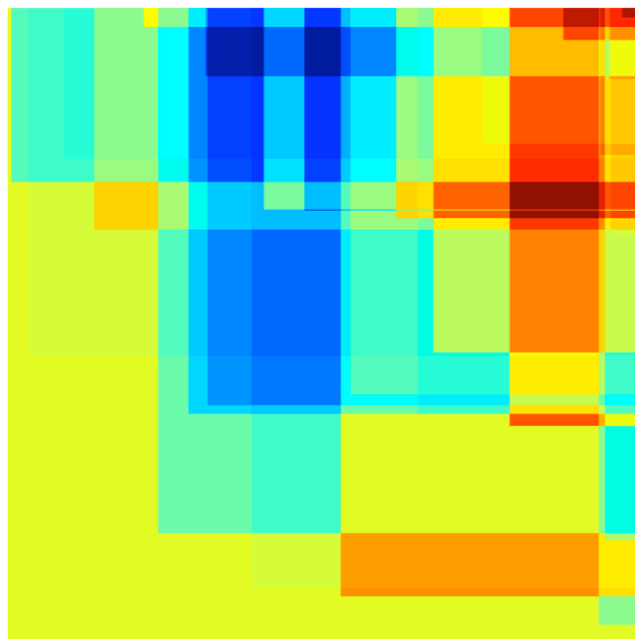
Fractional Brownian motion (Mandelbrot, 1968)

(U.-Tafti, *IEEE-SP* 2010)

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## Aesthetic sparse signal: the Mondrian process

$$L = D_x D_y \xleftrightarrow{\mathcal{F}} (j\omega_x)(j\omega_y)$$



$\lambda = 30$

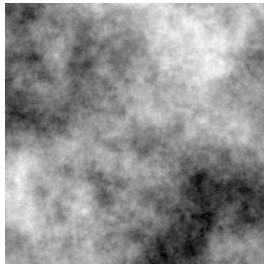
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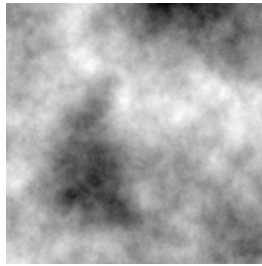
## Scale- and rotation-invariant processes

Stochastic partial differential equation :  $(-\Delta)^{\frac{H+1}{2}} s(\mathbf{x}) = w(\mathbf{x})$

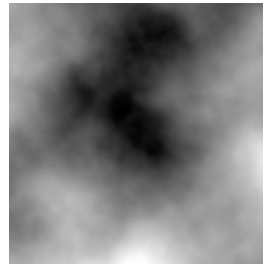
### Gaussian



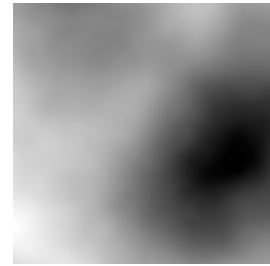
H=0.5



H=0.75

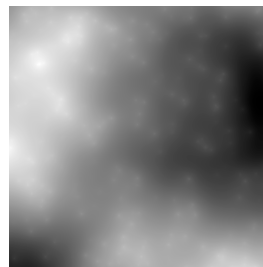
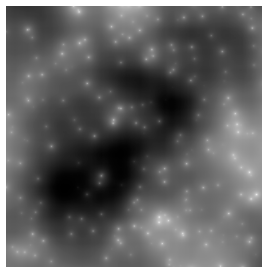
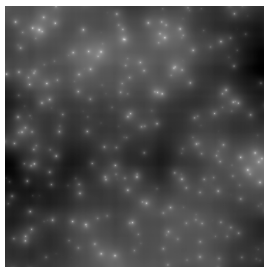


H=1.25



H=1.75

### Sparse (generalized Poisson)



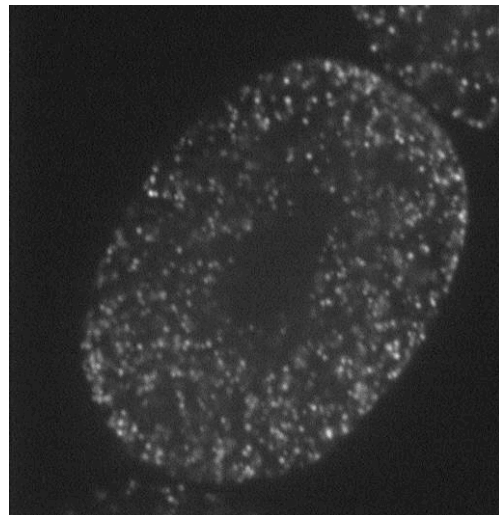
(U.-Tafti, *IEEE-SP* 2010)

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## Powers of ten: from astronomy to biology



© 1986 Jerry Lodriguss and John Martinez



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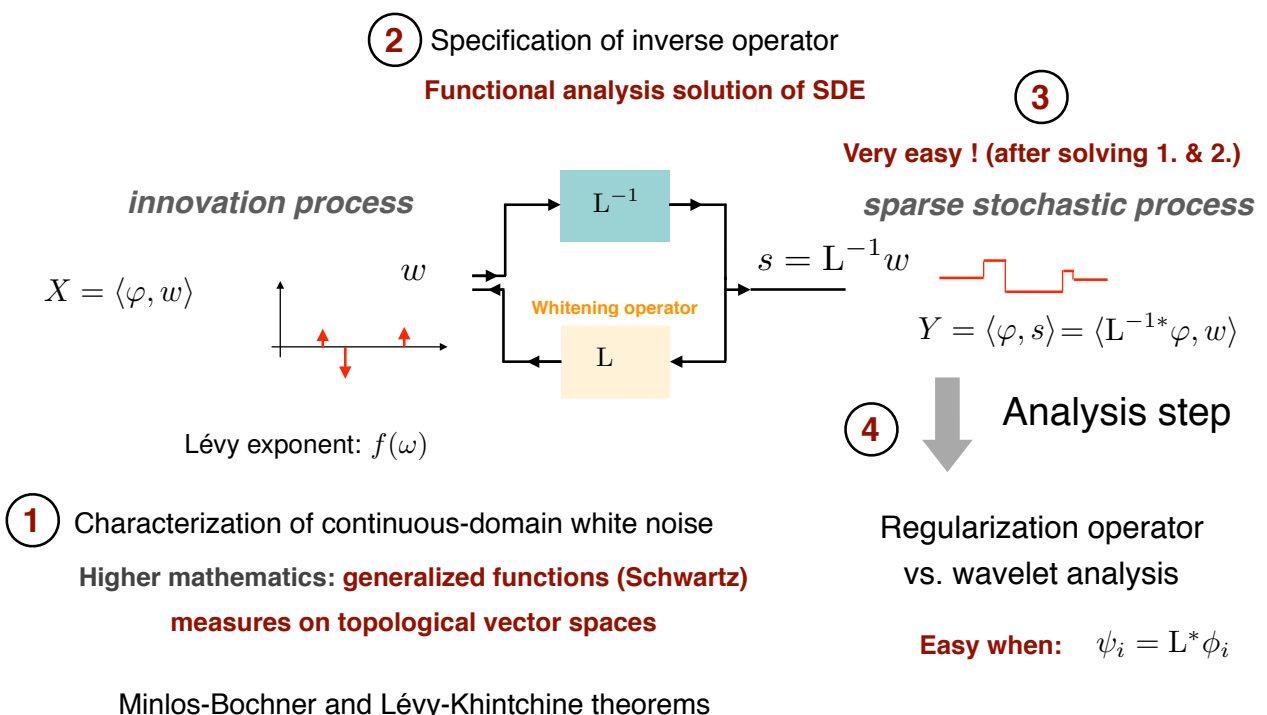
# PART II: RECOVERY OF SPARSE SIGNALS

- 10.1 Discretization of inverse problem
- 10.2 MAP estimation and regularization
- 10.3 MAP reconstruction of biomedical images
  - Deconvolution of fluorescent micrographs
  - Magnetic resonance imaging
  - X-ray tomography
- 10.4 Quest for minimum error solution

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## Generalized innovation model

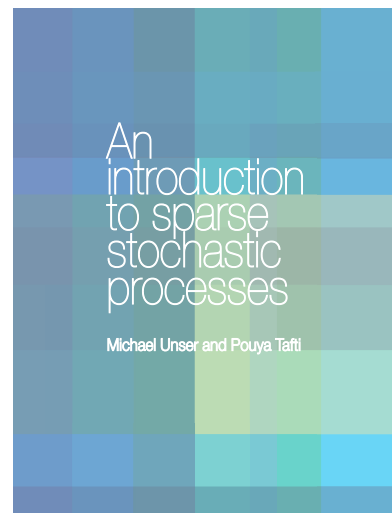
Theoretical framework: Gelfand's theory of generalized stochastic processes



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# Table of content

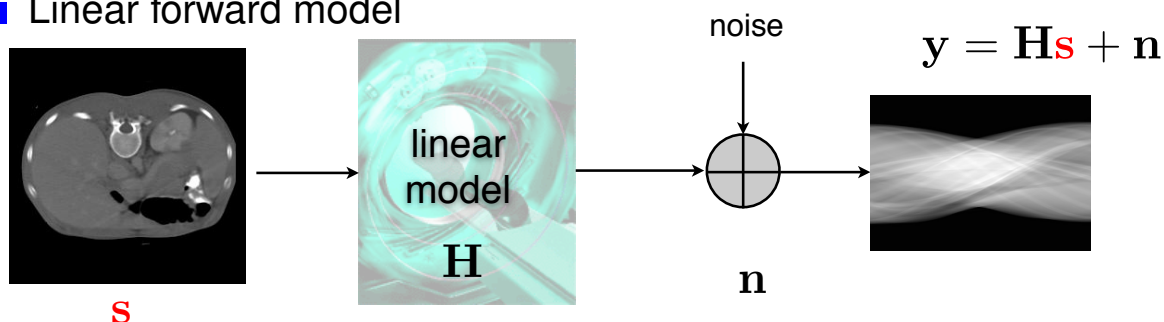
1. Introduction
2. **Roadmap to the monograph**
3. Mathematical context and background
4. **Continuous-domain innovation models**
5. Operators and their inverses
6. Splines and wavelets
7. **Sparse stochastic processes**
8. Sparse representations
9. Infinite divisibility and transform-domain statistic
10. **Recovery of sparse signals**
11. Wavelet-domain methods



<http://www.sparseprocesses.org/>

## Resolution of linear inverse problems

### ■ Linear forward model



Ill-posed inverse problem: recover  $\mathbf{s}$  from noisy measurements  $\mathbf{y}$

### ■ Reconstruction as an optimization problem

$$\mathbf{s}^* = \operatorname{argmin} \underbrace{\|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2}_{\text{data consistency}} + \underbrace{\lambda \mathcal{R}(\mathbf{s})}_{\text{regularization}}$$

Bayesian prior  $-\log p_S(\mathbf{s})$

Gaussian-noise likelihood  $-\log p_{Y|S}(\mathbf{n})$

## Recap on probability model

- Continuous-domain model:  $s = L^{-1}w$

$w = Ls$ : generalized white noise process with Lévy exponent  $f(\omega)$

Characteristic functional:  $\widehat{\mathcal{P}}_w(\varphi) = \mathbb{E}\{e^{j\langle\varphi, w\rangle}\} = \exp\left(\int_{\mathbb{R}^d} f(\varphi(\mathbf{r}))d\mathbf{r}\right)$

- Discretization:  $s(\mathbf{k}), \mathbf{k} \in \mathbb{Z}^d$  (sampled values)

Discrete approximation of whitening operator:  $L_d$

Discrete increment process:

$$u[\mathbf{k}] = L_d s(\mathbf{x})|_{\mathbf{x}=\mathbf{k}} = (\beta_L * w)(\mathbf{x})|_{\mathbf{x}=\mathbf{k}} = \langle \beta_L(\mathbf{k} - \cdot), w \rangle$$

Generalized B-spline:  $\beta_L(\mathbf{x}) = L_d L^{-1} \delta(\mathbf{x})$

- Statistical properties

-  $u[\mathbf{k}]$  are identically distributed and approximately independent

- **Infinitely divisible** with Lévy exponent  $f_U(\omega) = \log \widehat{p}_U(\omega) = \log \widehat{\mathcal{P}}_w(\omega \beta_L)$

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## Discretization of reconstruction problem

Spline-like reconstruction model:  $s(\mathbf{r}) = \sum_{\mathbf{k} \in \Omega} s[\mathbf{k}] \beta_{\mathbf{k}}(\mathbf{r}) \longleftrightarrow \mathbf{s} = (s[\mathbf{k}])_{\mathbf{k} \in \Omega}$

- Innovation model

$$\begin{aligned} Ls &= w \\ s &= L^{-1}w \end{aligned}$$

Discretization

$$\mathbf{u} = L\mathbf{s} \quad (\text{matrix notation})$$

$p_U$  is part of **infinitely divisible** family

- Physical model: image formation and acquisition

$$y_m = \int_{\mathbb{R}^d} s_1(\mathbf{x}) \eta_m(\mathbf{x}) d\mathbf{x} + n[m] = \langle s_1, \eta_m \rangle + n[m], \quad (m = 1, \dots, M)$$

$$\mathbf{y} = \mathbf{y}_0 + \mathbf{n} = \mathbf{H}\mathbf{s} + \mathbf{n}$$

$\mathbf{n}$ : i.i.d. noise with pdf  $p_N$

$$[\mathbf{H}]_{m,\mathbf{k}} = \langle \eta_m, \beta_{\mathbf{k}} \rangle = \int_{\mathbb{R}^d} \eta_m(\mathbf{r}) \beta_{\mathbf{k}}(\mathbf{r}) d\mathbf{r}: \quad (M \times K) \text{ system matrix}$$

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## Posterior probability distribution

$$p_{S|Y}(\mathbf{s}|\mathbf{y}) = \frac{p_{Y|S}(\mathbf{y}|\mathbf{s})p_S(\mathbf{s})}{p_Y(\mathbf{y})} = \frac{p_N(\mathbf{y} - \mathbf{H}\mathbf{s})p_S(\mathbf{s})}{p_Y(\mathbf{y})} \quad (\text{Bayes' rule})$$

$$= \frac{1}{Z} p_N(\mathbf{y} - \mathbf{H}\mathbf{s})p_S(\mathbf{s})$$

$$\mathbf{u} = \mathbf{L}\mathbf{s} \quad \Rightarrow \quad p_S(\mathbf{s}) \propto p_U(\mathbf{L}\mathbf{s})$$

$$p_{S|Y}(\mathbf{s}|\mathbf{y}) \propto p_N(\mathbf{y} - \mathbf{H}\mathbf{s})p_U(\mathbf{L}\mathbf{s}) \approx p_N(\mathbf{y} - \mathbf{H}\mathbf{s}) \prod_{\mathbf{k} \in \Omega} p_U([\mathbf{L}\mathbf{s}]_{\mathbf{k}})$$

(decoupling simplification)

- Additive white Gaussian noise scenario (AWGN)

$$p_{S|Y}(\mathbf{s}|\mathbf{y}) \propto \exp\left(-\frac{\|\mathbf{y} - \mathbf{H}\mathbf{s}\|^2}{2\sigma^2}\right) \prod_{\mathbf{k} \in \Omega} p_U([\mathbf{L}\mathbf{s}]_{\mathbf{k}})$$

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## Statement of MAP reconstruction problem

- Hypotheses

$\mathbf{y} = \mathbf{H}\mathbf{s} + \mathbf{n}$  where  $\mathbf{n}$  AWGN with variance  $\sigma^2$

$\mathbf{L}\mathbf{s} = \mathbf{u}$ : i.i.d. with pdf  $p_U$  and id potential function  $\Phi_U(x) = -\log p_U(x)$

- Maximum a posteriori (MAP) estimator

$$\mathbf{s}_{\text{MAP}} = \arg \min_{\mathbf{s} \in \mathbb{R}^K} \left( \frac{1}{2} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \sigma^2 \sum_{\mathbf{k} \in \Omega} \Phi_U([\mathbf{L}\mathbf{s}]_{\mathbf{k}}) \right)$$

- Gaussian:  $p_U(x) = \frac{1}{\sqrt{2\pi}\sigma_0} e^{-x^2/(2\sigma_0^2)} \quad \Rightarrow \quad \Phi_U(x) = \frac{1}{2\sigma_0^2} x^2 + C_1$
- Laplace:  $p_U(x) = \frac{\lambda}{2} e^{-\lambda|x|} \quad \Rightarrow \quad \Phi_U(x) = \lambda|x| + C_2$
- Student:  $p_U(x) = \frac{1}{B(r, \frac{1}{2})} \left( \frac{1}{x^2 + 1} \right)^{r+\frac{1}{2}} \quad \Rightarrow \quad \Phi_U(x) = \left(r + \frac{1}{2}\right) \log(1 + x^2) + C_3$

Sparser

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$p_X(x)$	$\Phi_X(x) = -\log p_X(x)$ as $x \rightarrow 0$	$\Phi_X(x)$ as $x \rightarrow \pm\infty$	Smooth	Convex
Gaussian	$a_0 + \frac{x^2}{2\sigma^2}$	$a_0 + \frac{x^2}{2\sigma^2}$	Yes	Yes
Laplace ( $\lambda \in \mathbb{R}^+$ )	$a_0 + \lambda x $	$a_0 + \lambda x $	No	Yes
Sym Gamma $r \in \mathbb{R}^+$	$\begin{cases} \log(a'_0 + a'_r x ^{2r-1} + O(x^2)), & r < 3/2 \\ a_0 + \frac{x^2}{4r-6} + O( x ^{\min(4, 2r-1)}), & r > 3/2 \end{cases}$	$b_0 +  x  - (r-1)\log x $	No	No
Hyperbolic secant	$a_0 + \frac{\pi^2 x^2}{8\sigma_0^2} + O(x^4)$	$-\log\sigma_0 + \frac{\pi}{2\sigma_0} x $	Yes	Yes
Meixner $r, s \in \mathbb{R}^+$	$a_0 + \frac{\psi^{(1)}(r/2)}{4s^2}x^2 + O(x^4)$	$b_0 + \frac{\pi}{2s} x  - (r-1)\log x $	Yes	No
Cauchy $s \in \mathbb{R}^+$	$a_0 + \frac{x^2}{s^2} + O(x^4)$	$b_0 - \log s + 2\log x $	Yes	No
Sym Student $r \in \mathbb{R}^+$	$a_0 + (r + \frac{1}{2})x^2 + O(x^4)$	$b_0 + (2r+1)\log x $	Yes	No
SaS, $\alpha \in (0, 2], s \in \mathbb{R}^+$	$a_0 + \frac{\Gamma(\frac{3}{\alpha})}{2s^2\Gamma(\frac{1}{\alpha})}x^2 + O(x^4)$	$b_0 - \alpha\log s + (\alpha+1)\log x $	Yes	No

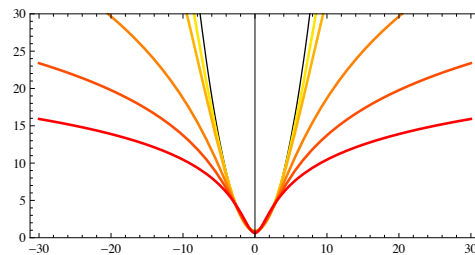
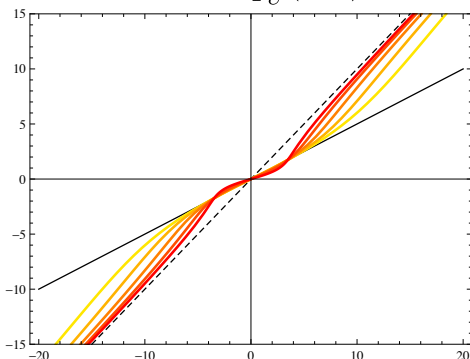
$\Gamma(z)$  and  $\psi^{(1)}(r)$  are Euler's gamma and first-order poly-gamma functions, respectively (see Appendix C).

**Table 10.1** Asymptotic behavior of the potential function  $\Phi_X(x)$  for the infinite-divisible distributions in Table 4.1.

## Proximal operators

$$\text{prox}_{\Phi_U}(y; \sigma^2) = \arg \min_{u \in \mathbb{R}} \frac{1}{2}|y - u|^2 + \sigma^2 \Phi_U(u)$$

$$\tilde{u} = \text{prox}_{\Phi_U}(y; 1)$$



Student potentials:  $r = 2, 4, 8, 32$  (fixed variance)

Solution of functional equation:  $-y + \tilde{u} + \sigma^2 \Phi'_U(\tilde{u}) = 0$

One-to-one mapping  $y \mapsto \tilde{u}$  when  $1 + \sigma^2 \Phi''_U(u) \geq 0$

$$\Rightarrow \tilde{u}(y) = (\text{Id} + \sigma^2 \Phi'_U)^{-1}(y)$$

## Proximal operators (Cont'd)

- Special cases:  $\Phi_1(u) = \lambda|u|$  (Laplace) and  $\Phi_2(u) = |u|^2/(2\sigma_0^2)$  (Gaussian)

$$T_1(y) = \text{prox}_{\Phi_1}(y; \sigma^2) = \text{sign}(y) (|y| - \lambda\sigma^2)_+ \quad \text{(soft-threshold)}$$

$$T_2(y) = \text{prox}_{\Phi_2}(y; \sigma^2) = \frac{\sigma_0^2}{\sigma_0^2 + \sigma^2} y \quad \text{(linear attenuation)}$$

### Asymptotics

Around origin when  $\Phi_U$  is twice differentiable

$$\Phi'_U(u) = \Phi''_U(0)u + O(u^2) \Rightarrow \text{prox}_{\Phi_U}(y; \sigma^2) = \frac{y}{1 + \sigma^2\Phi''_U(0)} \text{ as } y \rightarrow 0$$

Exponential and sub-exponential category:  $\lim_{u \rightarrow \infty} \Phi'_U(u) = b_1 + O(1/u)$

$$\text{prox}_{\Phi_U}(y; \sigma^2) \sim y - \sigma^2 b_1 \text{ as } y \rightarrow +\infty \quad \text{(shrinkage)}$$

Heavy-tailed category:  $\lim_{u \rightarrow \infty} \Phi'_U(u) = b_2/u$

$$\text{prox}_{\Phi_U}(y; \sigma^2) \sim y \text{ as } y \rightarrow \infty \quad \text{(identity)}$$

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## Maximum a posteriori (MAP) estimation

### Constrained optimization formulation

Auxiliary **innovation** variable:  $\mathbf{u} = \mathbf{L}\mathbf{s}$

$$\mathbf{s}_{\text{MAP}} = \arg \min_{\mathbf{s} \in \mathbb{R}^K} \left( \frac{1}{2} \|\mathbf{y} - \mathbf{H}\mathbf{s}\|_2^2 + \sigma^2 \sum_n \Phi_U([\mathbf{u}]_n) \right) \text{ subject to } \mathbf{u} = \mathbf{L}\mathbf{s}$$

### Augmented Lagrangian method

Quadratic penalty term:  $\frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2$

Lagrange multiplier vector:  $\boldsymbol{\alpha}$

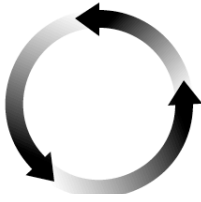
$$\mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}, \boldsymbol{\alpha}) = \frac{1}{2} \|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2 + \lambda \left( \sum_n \Phi_U([\mathbf{u}]_n) - \boldsymbol{\alpha}^T (\mathbf{L}\mathbf{s} - \mathbf{u}) + \frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2 \right)$$

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## Alternating direction method of multipliers (ADMM)

$$\mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}, \boldsymbol{\alpha}) = \frac{1}{2} \|\mathbf{g} - \mathbf{H}\mathbf{s}\|_2^2 + \lambda \left( \sum_n \Phi_U([\mathbf{u}]_n) - \boldsymbol{\alpha}^T (\mathbf{L}\mathbf{s} - \mathbf{u}) + \frac{\mu}{2} \|\mathbf{L}\mathbf{s} - \mathbf{u}\|_2^2 \right)$$

Sequential minimization



$$\mathbf{s}^{k+1} \leftarrow \arg \min_{\mathbf{s} \in \mathbb{R}^N} \mathcal{L}_{\mathcal{A}}(\mathbf{s}, \mathbf{u}^k, \boldsymbol{\alpha}^k)$$

$$\boldsymbol{\alpha}^{k+1} = \boldsymbol{\alpha}^k - \mu (\mathbf{L}\mathbf{s}^{k+1} - \mathbf{u}^k)$$

$$\mathbf{u}^{k+1} \leftarrow \arg \min_{\mathbf{u} \in \mathbb{R}^N} \mathcal{L}_{\mathcal{A}}(\mathbf{s}^{k+1}, \mathbf{u}, \boldsymbol{\alpha}^{k+1})$$

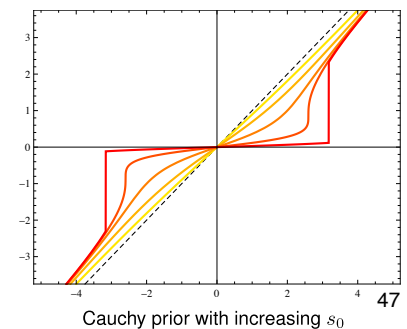
**Linear inverse problem:**  $\mathbf{s}^{k+1} = (\mathbf{H}^T \mathbf{H} + \mu \mathbf{L}^T \mathbf{L})^{-1} (\mathbf{H}^T \mathbf{y} + \mathbf{z}^{k+1})$

with  $\mathbf{z}^{k+1} = \mathbf{L}^T (\mu \mathbf{u}^{k+1} - \boldsymbol{\alpha})$

**Nonlinear denoising:**  $\mathbf{u}^{k+1} = \text{prox}_{\Phi_U}(\mathbf{L}\mathbf{s}^k + \boldsymbol{\alpha}^k; \lambda \mu^{-1})$

- Proximal operator tailored to stochastic model

$$\text{prox}_{\Phi_U}(y; \lambda) = \arg \min_u \frac{1}{2} |y - u|^2 + \lambda \Phi_U(u)$$



## 10.3 RECONSTRUCTION OF BIOMEDICAL IMAGES

- Common image model and numerical set-up

- $\frac{1}{|\boldsymbol{\omega}|^\gamma}$  spectral decay  $\longleftrightarrow (-\Delta)^{\frac{\gamma}{2}} s = w$  (self-similar image model)

- Robust localization/decoupling  $\mathbf{L}$ : discrete gradient magnitude (rotation invariant)

- Three flavors of potentials:

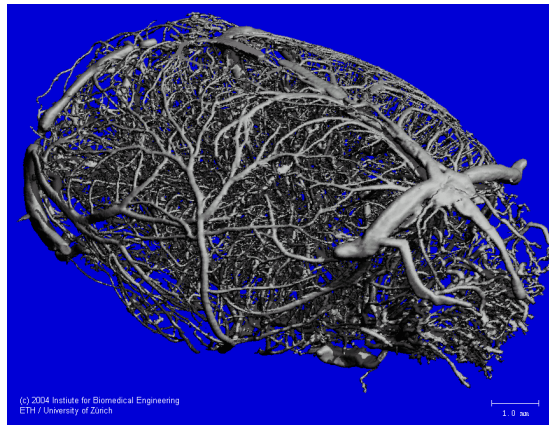
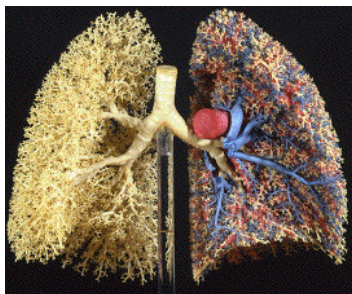
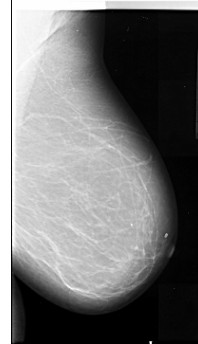
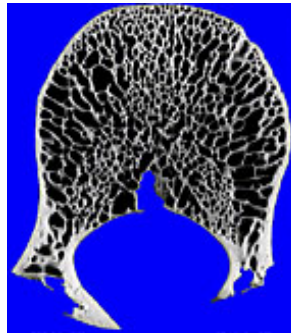
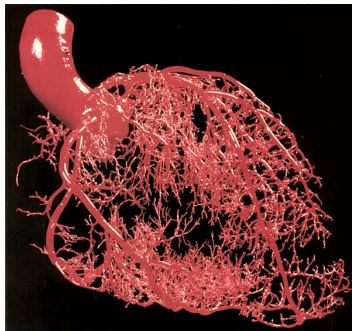
$$|x|^2 \text{ (Gaussian)}, |x| \text{ (Laplacian)}, \log(x^2 + \epsilon) \text{ (Student)}$$

- Deconvolution of fluorescent micrographs
- Magnetic resonance imaging
- X-ray tomography



# Relevance of self-similarity for bio-imaging

## ■ Fractals and physiology



(c) 2004 Institute for Biomedical Engineering  
ETH / University of Zurich

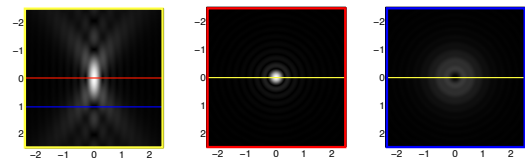
1.0 mm

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# Deconvolution of fluorescence micrographs

## ■ Physical model of a diffraction-limited microscope

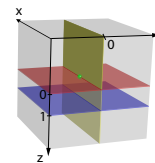
$$g(x, y, z) = (h_{3D} * s)(x, y, z)$$



### 3-D point spread function (PSF)

$$h_{3D}(x, y, z) = I_0 \left| p_\lambda \left( \frac{x}{M}, \frac{y}{M}, \frac{z}{M^2} \right) \right|^2$$

$$p_\lambda(x, y, z) = \int_{\mathbb{R}^2} P(\omega_1, \omega_2) \exp \left( j2\pi z \frac{\omega_1^2 + \omega_2^2}{2\lambda f_0^2} \right) \exp \left( -j2\pi \frac{x\omega_1 + y\omega_2}{\lambda f_0} \right) d\omega_1 d\omega_2$$



### Optical parameters

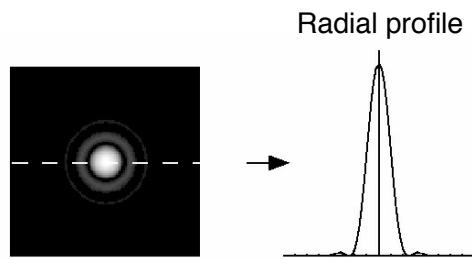
- $\lambda$ : wavelength (emission)
- $M$ : magnification factor
- $f_0$ : focal length
- $P(\omega_1, \omega_2) = \mathbb{1}_{\|\omega\| < R_0}$ : pupil function
- $\text{NA} = n \sin \theta = R_0 / f_0$ : numerical aperture

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## 2-D convolution model



- Airy disk:  $h_{2D}(x, y) = I_0 \left| 2 \frac{J_1(r/r_0)}{r/r_0} \right|^2$



with  $r = \sqrt{x^2 + y^2}$ ,  $r_0 = \frac{\lambda f_0}{2\pi R_0}$ ,  $J_1(r)$ : first-order Bessel function.

- Modulation transfer function

$$\hat{h}_{2D}(\boldsymbol{\omega}) = \begin{cases} \frac{2}{\pi} \left( \arccos\left(\frac{\|\boldsymbol{\omega}\|}{\omega_0}\right) - \frac{\|\boldsymbol{\omega}\|}{\omega_0} \sqrt{1 - \left(\frac{\|\boldsymbol{\omega}\|}{\omega_0}\right)^2} \right), & \text{for } 0 \leq \|\boldsymbol{\omega}\| < \omega_0 \\ 0, & \text{otherwise} \end{cases}$$

Cut-off frequency (Rayleigh):  $\omega_0 = \frac{2R_0}{\lambda f_0} = \frac{\pi}{r_0} \approx \frac{2NA}{\lambda}$

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## 2-D deconvolution: numerical set-up

- Discretization

$\omega_0 \leq \pi$  and representation in (separable) sinc basis  $\{\text{sinc}(\mathbf{x} - \mathbf{k})\}_{\mathbf{k} \in \mathbb{Z}^2}$

Analysis functions:  $\eta_{\mathbf{m}}(x, y) = h_{2D}(x - m_1, y - m_2)$

$$\begin{aligned} [\mathbf{H}]_{\mathbf{m}, \mathbf{k}} &= \langle \eta_{\mathbf{m}}, \text{sinc}(\cdot - \mathbf{k}) \rangle \\ &= \langle h_{2D}(\cdot - \mathbf{m}), \text{sinc}(\cdot - \mathbf{k}) \rangle \\ &= (\text{sinc} * h_{2D})(\mathbf{m} - \mathbf{k}) = h_{2D}(\mathbf{m} - \mathbf{k}). \end{aligned}$$

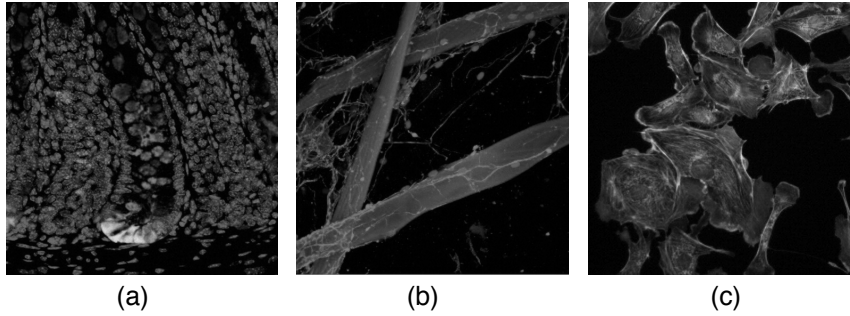
$\mathbf{H}$  and  $\mathbf{L}$ : convolution matrices diagonalized by discrete Fourier transform

- Linear step of ADMM algorithm implemented using the FFT

$$\begin{aligned} \mathbf{s}^{k+1} &= (\mathbf{H}^T \mathbf{H} + \mu \mathbf{L}^T \mathbf{L})^{-1} (\mathbf{H}^T \mathbf{y} + \mathbf{z}^{k+1}) \\ &\text{with } \mathbf{z}^{k+1} = \mathbf{L}^T (\mu \mathbf{u}^{k+1} - \boldsymbol{\alpha}) \end{aligned}$$

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## Deconvolution experiments



**Figure 10.3** Images used in deconvolution experiments. (a) Stem cells surrounded by goblet cells. (b) Nerve cells growing around fibers. (c) Artery cells.

**Table 10.2** Deconvolution performance of MAP estimators based on different prior distributions.

	BSNR (dB)	Estimation performance (SNR in dB)		
		Gaussian	Laplace	Student's
Stem cells	20	<b>14.43</b>	13.76	11.86
	30	<b>15.92</b>	15.77	13.15
	40	<b>18.11</b>	<b>18.11</b>	13.83
Nerve cells	20	13.86	<b>15.31</b>	14.01
	30	15.89	<b>18.18</b>	15.81
	40	18.58	<b>20.57</b>	16.92
Artery cells	20	14.86	<b>15.23</b>	13.48
	30	16.59	<b>17.21</b>	14.92
	40	18.68	<b>19.61</b>	15.94

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## Magnetic resonance imaging (MRI)

- Physical image formation model (noise-free)

$$\hat{s}(\boldsymbol{\omega}_m) = \int_{\mathbb{R}^2} s(\mathbf{r}) e^{-j\langle \boldsymbol{\omega}_m, \mathbf{r} \rangle} d\mathbf{r} \quad (\text{sampling of Fourier transform})$$

Equivalent analysis function:  $\eta_m(\mathbf{r}) = e^{-j\langle \boldsymbol{\omega}_m, \mathbf{r} \rangle}$

- Discretization in separable sinc basis

$$\begin{aligned} [\mathbf{H}]_{m,\mathbf{n}} &= \langle \eta_m, \text{sinc}(\cdot - \mathbf{n}) \rangle \\ &= \langle e^{-j\langle \boldsymbol{\omega}_m, \cdot \rangle}, \text{sinc}(\cdot - \mathbf{n}) \rangle = e^{-j\langle \boldsymbol{\omega}_m, \mathbf{n} \rangle} \end{aligned}$$

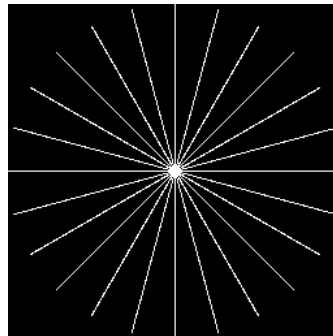
Property:  $\mathbf{H}^T \mathbf{H}$  is circulant (FFT-based implementation)

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## MRI: Shepp-Logan phantom



Original SL Phantom



Fourier Sampling Pattern  
12 Angles



Laplace prior (TV)



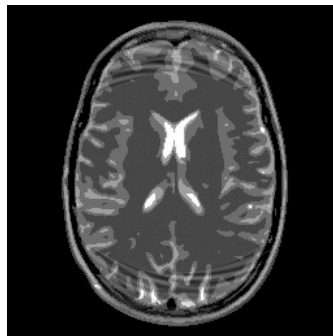
Student prior (log)

L : gradient  
Optimized parameters

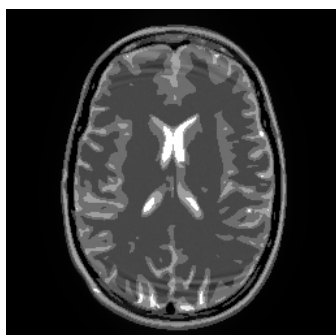
## MRI phantom: Spiral sampling in k-space



Original Phantom  
(Guerquin-Kern TMI 2012)



Gaussian prior (Tikhonov)  
SER = 17.69 dB



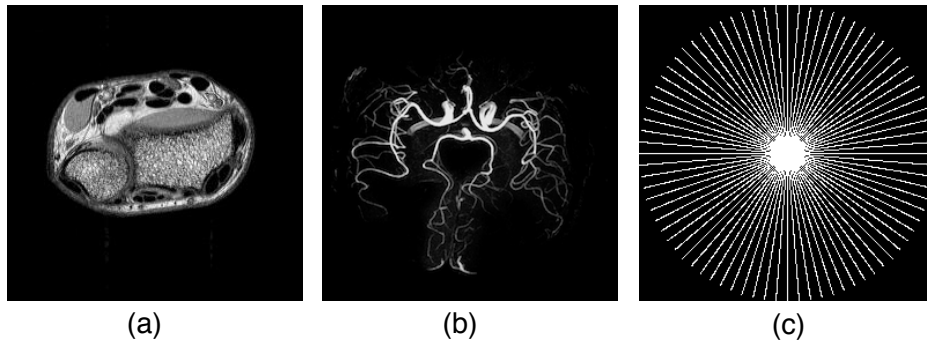
Laplace prior (TV)  
SER = 21.37 dB



Student prior  
SER = 27.22 dB

L : gradient  
Optimized parameters

# MRI reconstruction experiments



**Figure 10.4** Data used in MR reconstruction experiments. (a) Cross section of a wrist. (b) Angiography image. (c) k-space sampling pattern along 40 radial lines.

**Table 10.3** MR reconstruction performance of MAP estimators based on different prior distributions.

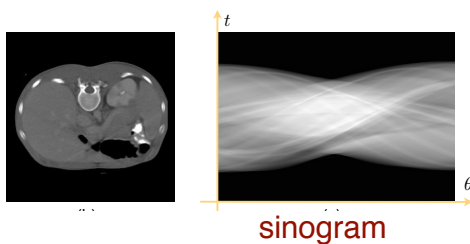
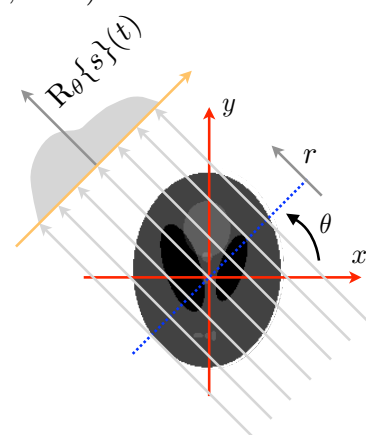
	Radial lines	Estimation performance (SNR in dB)		
		Gaussian	Laplace	Student's
Wrist	20	8.82	<b>11.8</b>	5.97
	40	11.30	<b>14.69</b>	13.81
Angiogram	20	4.30	9.01	<b>9.40</b>
	40	6.31	14.48	<b>14.97</b>

# X-ray tomography

Projection geometry:  $\mathbf{x} = t\boldsymbol{\theta} + r\boldsymbol{\theta}^\perp$  with  $\boldsymbol{\theta} = (\cos \theta, \sin \theta)$

■ Radon transform (line integrals)

$$\begin{aligned} R_\theta\{s(\mathbf{x})\}(t) &= \int_{\mathbb{R}} s(t\boldsymbol{\theta} + r\boldsymbol{\theta}^\perp) dr \\ &= \int_{\mathbb{R}^2} s(\mathbf{x}) \delta(t - \langle \mathbf{x}, \boldsymbol{\theta} \rangle) d\mathbf{x} \end{aligned}$$



Equivalent analysis functions:  $\eta_m(\mathbf{x}) = \delta(t_m - \langle \mathbf{x}, \boldsymbol{\theta}_m \rangle)$

# Properties of Radon transform

- Projected translation invariance

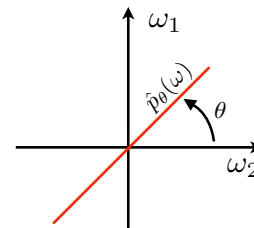
$$\mathbf{R}_\theta\{\varphi(\cdot - \mathbf{x}_0)\}(t) = \mathbf{R}_\theta\{\varphi\}(t - \langle \mathbf{x}_0, \boldsymbol{\theta} \rangle)$$



- Pseudo-distributivity with respect to convolution

$$\mathbf{R}_\theta\{\varphi_1 * \varphi_2\}(t) = (\mathbf{R}_\theta\{\varphi_1\} * \mathbf{R}_\theta\{\varphi_2\})(t)$$

$$\hat{p}_\theta(\omega) = \widehat{\mathbf{R}_\theta\{\varphi\}}(\omega) = \hat{\varphi}(\omega \cos \theta, \omega \sin \theta)$$



- Fourier central-slice theorem

$$\int_{\mathbb{R}} \mathbf{R}_\theta\{\varphi\}(t) e^{-j\omega t} dt = \hat{\varphi}(\omega)|_{\omega=\omega\theta}$$

**Proposition:** Consider the separable function  $\varphi(\mathbf{x}) = \varphi_1(x)\varphi_2(y)$ . Then,

$$\mathbf{R}_\theta\{\varphi(\cdot - \mathbf{x}_0)\}(t) = \varphi_\theta(t - t_0)$$

where  $t_0 = \langle \mathbf{x}_0, \boldsymbol{\theta} \rangle$  and

$$\varphi_\theta(t) = \left( \frac{1}{|\cos \theta|} \varphi_1\left(\frac{\cdot}{\cos \theta}\right) * \frac{1}{|\sin \theta|} \varphi_2\left(\frac{\cdot}{\sin \theta}\right) \right)(t).$$

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# Discretization using polynomial B-splines

- Separable B-spline reconstruction model

$$s(\mathbf{x}) = \sum_{\mathbf{k}} s[\mathbf{k}] \beta^n(\mathbf{x} - \mathbf{k}) \quad \text{with} \quad \beta^n(\mathbf{x}) = \beta^n(x) \beta^n(y)$$

Centered polynomial B-spline: 
$$\beta^n(x) = \sum_{k=0}^{n+1} (-1)^k \binom{n+1}{k} \frac{(x - k + \frac{n+1}{2})_+^n}{n!}$$

- Radon transform of B-spline

$$\mathbf{R}_\theta\{\beta^n(x)\beta^n(y)\}(t) = \beta_\theta^n(t)$$

$$= \sum_{k=0}^{n+1} \sum_{k'=0}^{n+1} (-1)^{k+k'} \binom{n+1}{k} \binom{n+1}{k'} \frac{(t + (\frac{n+1}{2} - k) \cos \theta + (\frac{n+1}{2} - k') \sin \theta)_+^{2n+1}}{|\cos \theta|^{n+1} |\sin \theta|^{n+1} (2n+1)!}$$

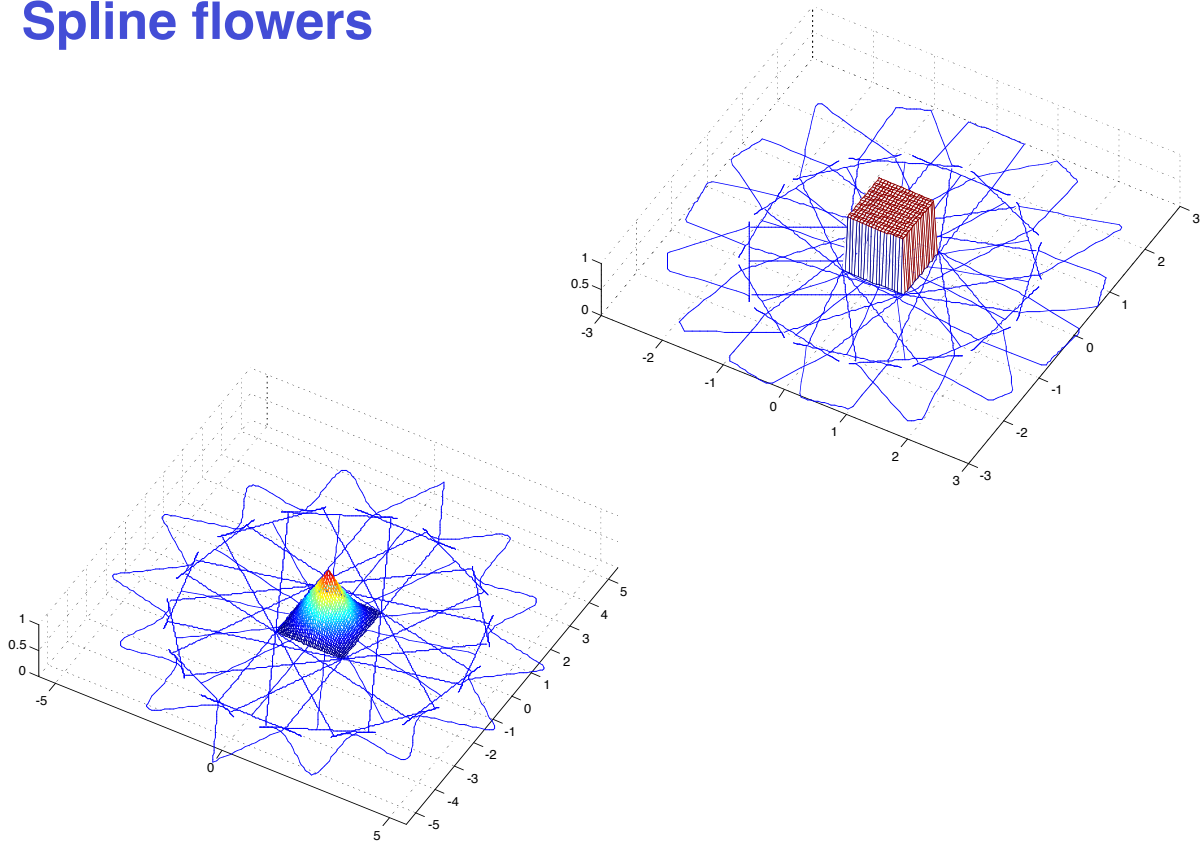
Justification: 
$$\frac{t_+^{n_1}}{n_1!} * \frac{t_+^{n_2}}{n_2!} = \frac{t_+^{n_1+n_2+1}}{(n_1+n_2+1)!}$$

- System matrix  $[\mathbf{H}]_{m,\mathbf{k}} = \langle \delta(t_m - \langle \cdot, \boldsymbol{\theta}_m \rangle), \beta^n(\cdot - \mathbf{k}) \rangle$

$$= \mathbf{R}_{\boldsymbol{\theta}_m}\{\beta^n(\cdot - \mathbf{k})\}(t_m) = \beta_{\boldsymbol{\theta}_m}^n(t_m - \langle \mathbf{k}, \boldsymbol{\theta}_m \rangle)$$

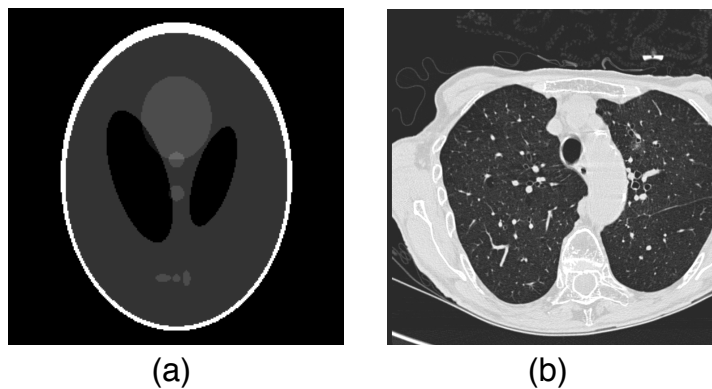
60

## Spline flowers



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## X-ray tomography reconstruction results



**Figure 10.6** Images used in X-ray tomographic reconstruction experiments. (a) The Shepp-Logan (SL) phantom. (b) Cross section of a human lung.

**Table 10.4** Reconstruction results of X-ray computed tomography using different estimators.

	Directions	Estimation performance (SNR in dB)		
		Gaussian	Laplace	Student's
SL Phantom	120	16.8	17.53	<b>18.76</b>
SL Phantom	180	18.13	18.75	<b>20.34</b>
Lung	180	<b>22.49</b>	21.52	21.45
Lung	360	<b>24.38</b>	22.47	22.37

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## 10.4 QUEST FOR MINIMUM ERROR SOLUTION

### How suitable are MAP estimators ?

⇒ A detailed investigation of simpler denoising problem

- MMSE estimators for first-order processes
- Direct solution by belief propagation
- MMSE vs. MAP denoising of Lévy processes

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## MMSE estimators for first-order processes

Task: Recovery of non-Gaussian AR(1) and Lévy processes from noisy samples

- Measurement model:  $p_{(Y_1:Y_N|X_1:X_N)}(\mathbf{y}|\mathbf{x}) = \prod_{n=1}^N \underbrace{p_{Y|X}(y_n|x_n)}_{\text{independent noise contributions}}$

- Discrete innovation model:  $u_n = x_n - a_1 x_{n-1}$ ,  $u$  i.i.d. with pdf  $p_U$

- Posterior distribution of signal

$$p_{(X_1:X_N|Y_1:Y_N)}(\mathbf{x}|\mathbf{y}) = \frac{1}{Z} \prod_{n=1}^N p_{Y|X}(y_n|x_n) \prod_{n=1}^N p_U(\underbrace{x_n - a_1 x_{n-1}}_{u_n})$$

- Signal estimators

$$\mathbf{x}_{\text{MAP}}(\mathbf{y}) = \arg \max_{\mathbf{x} \in \mathbb{R}^N} \{p_{(X_1:X_N|Y_1:Y_N)}(\mathbf{x}|\mathbf{y})\}$$

$$\mathbf{x}_{\text{MMSE}}(\mathbf{y}) = \mathbb{E}\{\mathbf{x}|\mathbf{y}\} = \int_{\mathbb{R}^N} \mathbf{x} p_{(X_1:X_N|Y_1:Y_N)}(\mathbf{x}|\mathbf{y}) d\mathbf{x} \quad : \text{optimal MMSE solution}$$

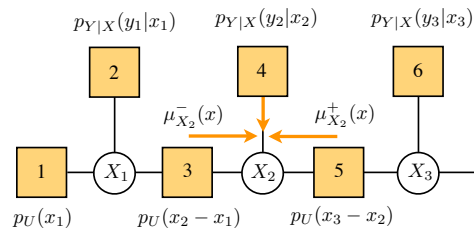
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# Introduction to BP algorithm

## ■ Estimation of a three-point Lévy process

$$p_{(X_1: X_3 | Y_1: Y_3)}(\mathbf{x} | \mathbf{y}) \propto p_U(x_1) p_{Y|X}(y_1 | x_1) p_U(x_2 - x_1) p_{Y|X}(y_2 | x_2) p_U(x_3 - x_2) p_{Y|X}(y_3 | x_3)$$



## ■ Recursive evaluation of marginal distributions

$$p_{(X_2 | Y_1: Y_3)}(x_2 | \mathbf{y}) = \int_{\mathbb{R}} \int_{\mathbb{R}} p_{(X_1: X_3 | Y_1: Y_3)}(\mathbf{x} | \mathbf{y}) dx_1 dx_3 \propto \underbrace{\int_{\mathbb{R}} \overbrace{p_U(x_1) p_{Y|X}(y_1 | x_1) p_U(x_2 - x_1)}^{\mu_{X_1}^-(x_1)} dx_1}_{\mu_{X_2}^-(x_2)} \cdot p_{Y|X}(y_2 | x_2) \cdot \underbrace{\int_{\mathbb{R}} p_U(x_3 - x_2) p_{Y|X}(y_3 | x_3) \cdot \overbrace{1}^{\mu_{X_3}^+(x_3)} dx_3}_{\mu_{X_2}^+(x_2)}$$

$$p_{(X_3 | Y_1: Y_3)}(x_3 | \mathbf{y}) = \int_{\mathbb{R}} \int_{\mathbb{R}} p_{(X_1: X_3 | Y_1: Y_3)}(\mathbf{x} | \mathbf{y}) dx_1 dx_2 \propto \underbrace{\int_{\mathbb{R}} \mu_{X_2}^-(x_2) p_{Y|X}(y_2 | x_2) p_U(x_3 - x_2) dx_2}_{\mu_{X_3}^-(x_3)} \cdot p_{Y|X}(y_3 | x_3) \cdot \underbrace{1}_{\mu_{X_3}^+(x_3)}$$

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# Direct MMSE solution by belief propagation

Factorized representation:  $p_{(X_n | Y_1: Y_N)}(x_n | \mathbf{y}) = \mu_{X_n}^-(x_n) \cdot p_{Y|X}(y_n | x_n) \cdot \mu_{X_n}^+(x_n)$

Auxiliary **belief** functions  $\mu_{X_n}^-(x)$  and  $\mu_{X_n}^+(x)$

## ■ BP for Lévy and non-Gaussian AR(1) processes

– Initialization: Set

$$\mu_{X_1}^-(x) = p_U(x) \\ \mu_{X_N}^+(x) = 1$$

– Forward message recursion: For  $n = 2$  to  $N$ , compute

$$\mu_{X_n}^-(x) \propto \int_{\mathbb{R}} \mu_{X_{n-1}}^-(z) p_{Y|X}(y_{n-1} | z) p_U(x - a_1 z) dz$$

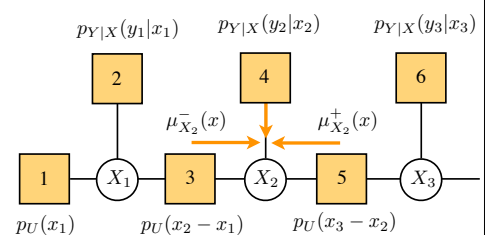
– Backward message recursion: For  $n = (N - 1)$  down to 1, compute

$$\mu_{X_n}^+(x) \propto \int_{\mathbb{R}} p_U(z - a_1 x) p_{Y|X}(y_{n+1} | z) \mu_{X_{n+1}}^+(z) dz$$

– Results: For  $n = 1$  to  $N$ , compute

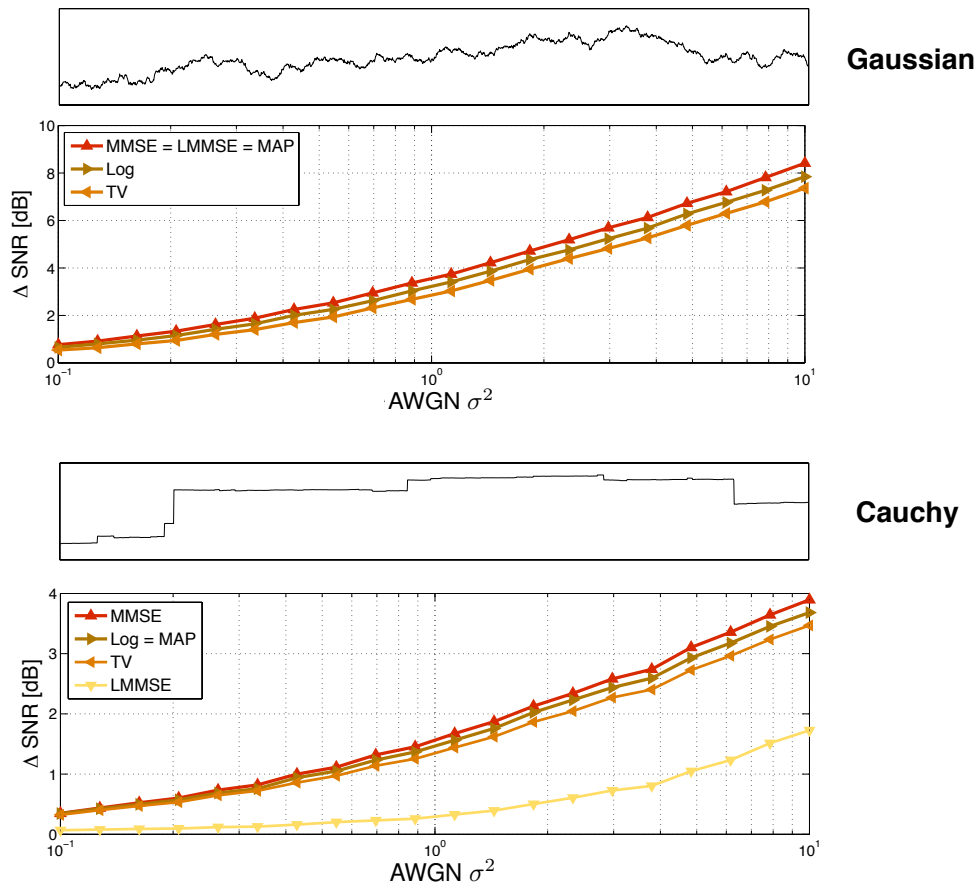
$$p_{(X_n | Y_1: Y_N)}(x | \mathbf{y}) \propto \mu_{X_n}^-(x) \cdot p_{Y|X}(y_n | x) \cdot \mu_{X_n}^+(x)$$

$$[\mathbf{x}_{\text{MMSE}}]_n = \int_{\mathbb{R}} x p_{(X_n | Y_1: Y_N)}(x | \mathbf{y}) dx$$



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## Experiment: Denoising of Lévy processes



## CONCLUSION

- Unifying continuous-domain stochastic model
  - Backward compatibility with classical Gaussian theory
  - Operator-based formulation: Lévy-driven SDEs or SPDEs
  - **Gaussian** vs. **sparse** (generalized Poisson, student,  $S\alpha S$ )
- Regularization
  - Sparsification via “operator-like” behavior (whitening)
  - Specific family of id potential functions (typ., non-convex)
- Conceptual framework for sparse signal recovery
  - New statistically-founded sparsity priors
  - Derivation of optimal estimators (MAP, MMSE)
  - Principled approach for the development of novel algorithms
- Challenges
  - Calculation of MMSE solution (belief propagation ?)
  - Fast algorithms for solving large scale inverse problems with (more or less) structure

## References

### ■ Theory of sparse stochastic processes

- M. Unser and P. Tafti, ***An Introduction to Sparse Stochastic Processes***, Cambridge University Press, 2014; preprint, available at <http://www.sparseprocesses.org>.
- M. Unser, P.D. Tafti, "Stochastic models for sparse and piecewise-smooth signals", *IEEE Trans. Signal Processing*, vol. 59, no. 3, pp. 989-1006, March 2011.
- M. Unser, P. Tafti, and Q. Sun, "A unified formulation of Gaussian vs. sparse stochastic processes—Part I: Continuous-domain theory," *IEEE Trans. Information Theory*, vol. 60, no. 3, pp. 1945-1962, March 2014.

### ■ Algorithms and imaging applications

- E. Bostan, U.S. Kamilov, M. Nilchian, M. Unser, "Sparse Stochastic Processes and Discretization of Linear Inverse Problems," *IEEE Trans. Image Processing*, vol. 22, no. 7, pp. 2699-2710, 2013.
- C. Vonesch, M. Unser, "A Fast Multilevel Algorithm for Wavelet-Regularized Image Restoration," *IEEE Trans. Image Processing*, vol. 18, no. 3, pp. 509-523, March 2009.
- M. Guerquin-Kern, M. Häberlin, K.P. Pruessmann, M. Unser, "A Fast Wavelet-Based Reconstruction Method for Magnetic Resonance Imaging," *IEEE Trans. Medical Imaging*, vol. 30, no. 9, pp. 1649-1660, 2011.
- U. Kamilov, P. Pad, A. Amini, M. Unser, "MMSE Estimation of Sparse Lévy Processes," *IEEE Trans. Signal Processing*, vol. 61, no. 1, pp. 137-147, January 1, 2013.

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- Ulugbek Kamilov
- Masih Nilchian



- **Members of EPFL's Biomedical Imaging Group**



- Preprints and demos: <http://bigwww.epfl.ch/>

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